



# Tensor decomposition exploiting structural constraints for brain source imaging

**Ahmad Karfoul**

joint work with

Hanna Becker, Laurent Albera,  
Rémi Gribonval, Julien Fleureau, Philippe Guillotel,  
Amar Kachenoura, Lotfi Senhadji, Isabelle Merlet

**One-Day workshop on tensors and  
covariance matrix estimation**

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**EEG and MEG:**  
Multisensor systems that record brain activity with a high temporal resolution



[www.canada-meg-consortium.org](http://www.canada-meg-consortium.org)

- ❑ **Objective:** Separation and localization of brain sources
- ❑ **Applications:**
  - Diagnosis and management of diseases such as epilepsy  
⇒ e.g., identification of epileptogenic zones
  - Neuroscience: Understanding of brain functions

## □ Tensor-based approaches for EEG source separation:

Exploited dimensions in addition to space and time:

- frequency [1]
- wave vector [2]
- subject [3]
- realization [4]

Employed tensor model:

- Canonical Polyadic (CP) decomposition [1,2]
- PARAFAC2 [5]
- Shift-invariant CP (SCP) [6]
- Block term decomposition [7]

[1] Miwakeichi et al. 2004

[2] Becker et al. 2012

[3] Morup et al. 2006

[4] Deburchgraeve et al. 2009

[5] Weis et al. 2010

[6] Morup et al. 2008

[7] Hunyadi et al. 2014

## □ Tensor-based approaches for EEG source separation:

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⇒ Tensor decomposition results are mostly used to identify spatial maps and time signals of the sources

- **Idea:** improve interpretation of EEG by identifying the source positions and their spatial extents → brain source imaging

## **1. Motivation**

## **2. Data Model**

## **3. CP Tensor decomposition**

## **4. Tensor - based source localization**

- **Classical two-steps approach**
- **Proposed single - step approach**

## **5. Simulations**

## **6. Conclusion**

## 2. Data model

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$$\mathbf{X} = \mathbf{G} \cdot \mathbf{S} \in \mathbb{R}^{N \times T}$$

$$\mathbf{G} \in \mathbb{R}^{N \times D}$$

$$\mathbf{S} \in \mathbb{R}^{D \times T}$$



- Lead field matrix: depends on spatial parameters

$N$  - number of sensors

- Signal matrix: temporal behavior of  $D$  dipoles

$T$  - number of time samples

## 2. Data model

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□ EEG data matrix:  $\mathbf{X} = \mathbf{G} \cdot \mathbf{S} \in \mathbb{R}^{N \times T}$

$\mathbf{G} \in \mathbb{R}^{N \times D}$

$\mathbf{S} \in \mathbb{R}^{D \times T}$



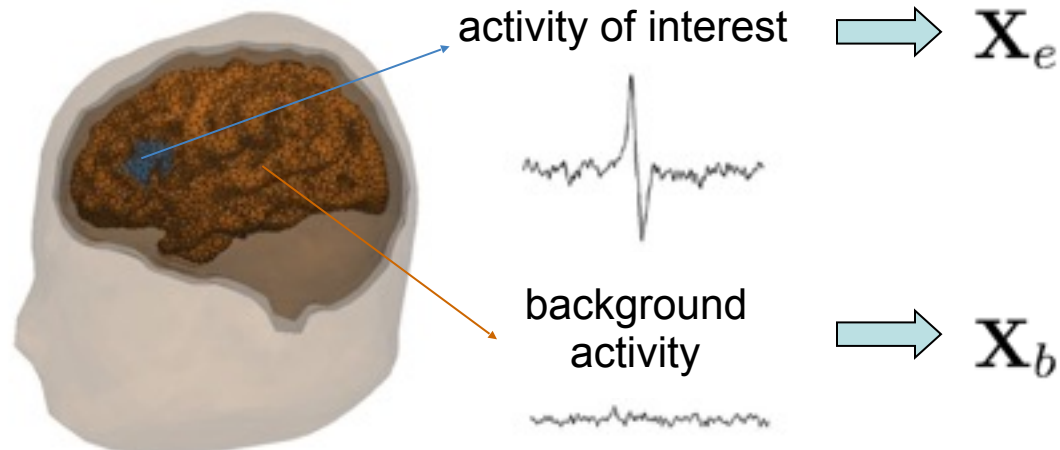
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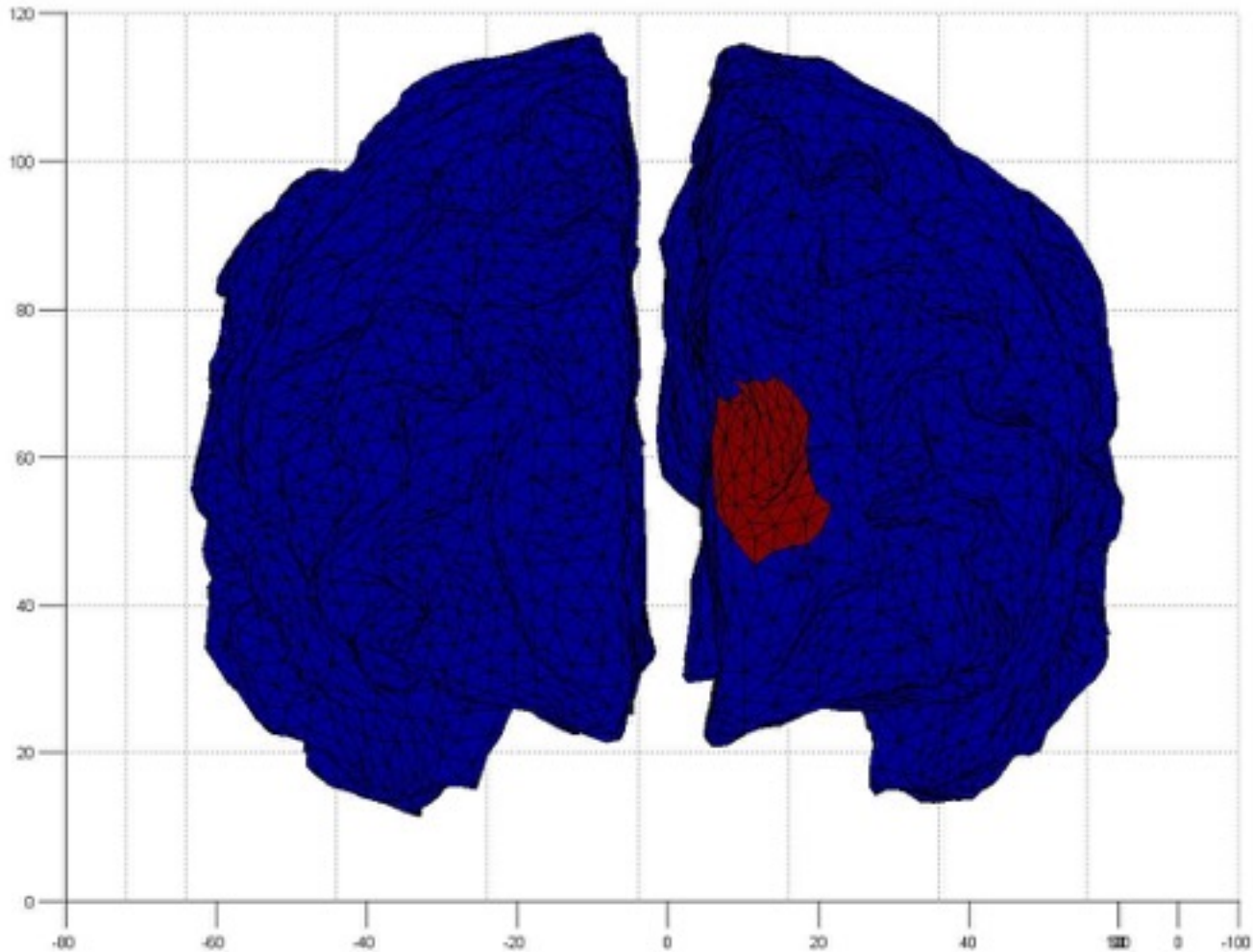
$T$  - number of time samples

- Distributed source model:



## 2.1 Example of a patch

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## 2. Data model

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□ EEG data matrix:  $\mathbf{X} = \mathbf{G} \cdot \mathbf{S} \in \mathbb{R}^{N \times T}$

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- Lead field matrix: depends on spatial parameters

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- Distributed source model:

$$\mathbf{X} = \mathbf{X}_e + \mathbf{X}_b = \sum_{p=1}^P \mathbf{h}_p \mathbf{s}_p^T + \mathbf{X}_b$$

$P$  - number of sources

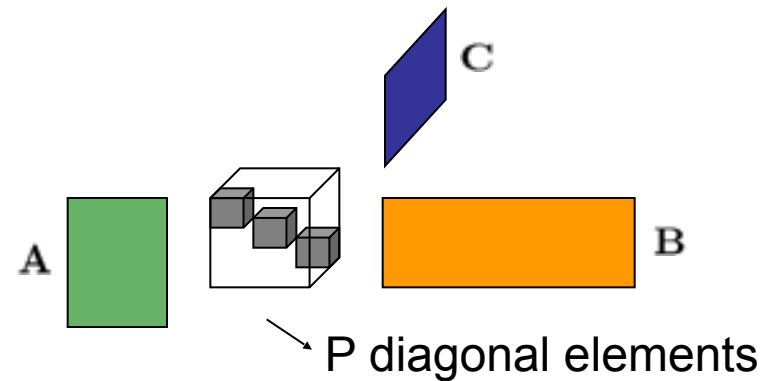
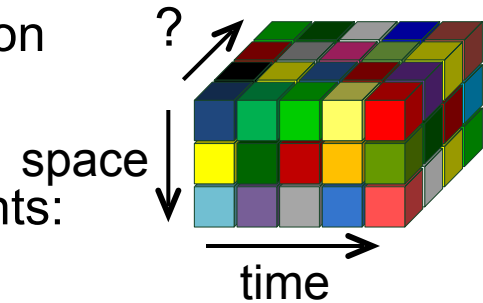
$\mathbf{h}_p = \mathbf{G}\psi_p$  distributed source lead field vector

$\psi_p$  - coefficient vector

average signal of the  $p$ -th source

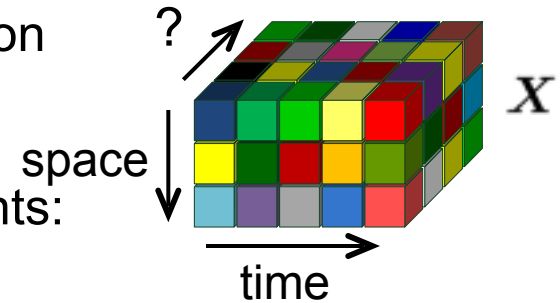
# 3. CP tensor decomposition

- Essentially unique (up to scale and permutation indeterminacies) under mild conditions
- Approximates a tensor by  $P$  rank-1 components:



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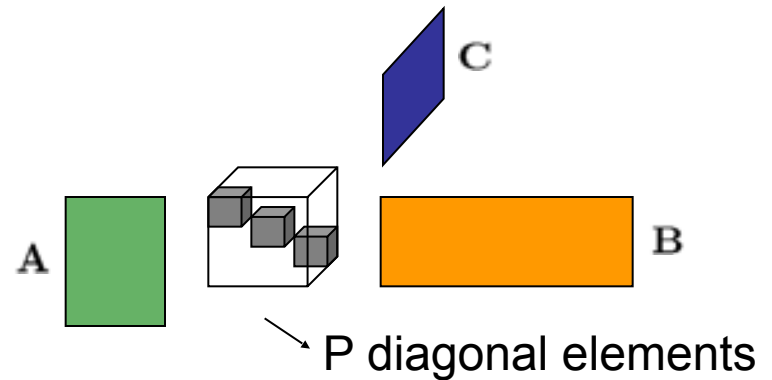
- Essentially unique (up to scale and permutation indeterminacies) under mild conditions
- Approximates a tensor by  $P$  rank-1 components:



$$X \approx \sum_{p=1}^P \mathbf{a}(p) \circ \mathbf{b}(p) \circ \mathbf{c}(p)$$



$$X \approx I \times_1 \mathbf{A} \times_2 \mathbf{B} \times_3 \mathbf{C}$$



# 3.1 Space-Time-Frequency (STF) analysis

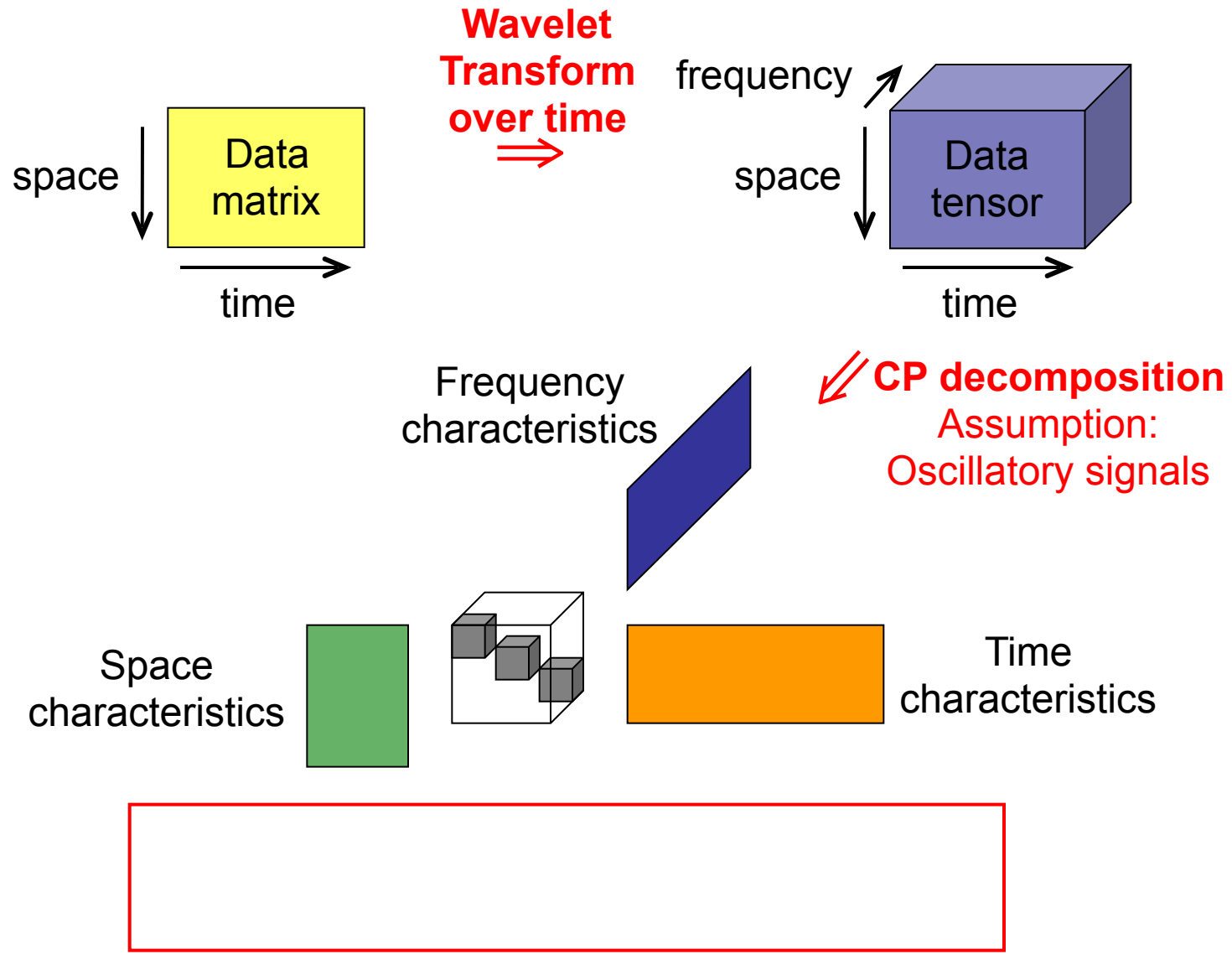


$$W(\mathbf{r}, t, f) = \int_{-\infty}^{\infty} x(\mathbf{r}, \tau) \cdot \psi(a, \tau, t) d\tau$$

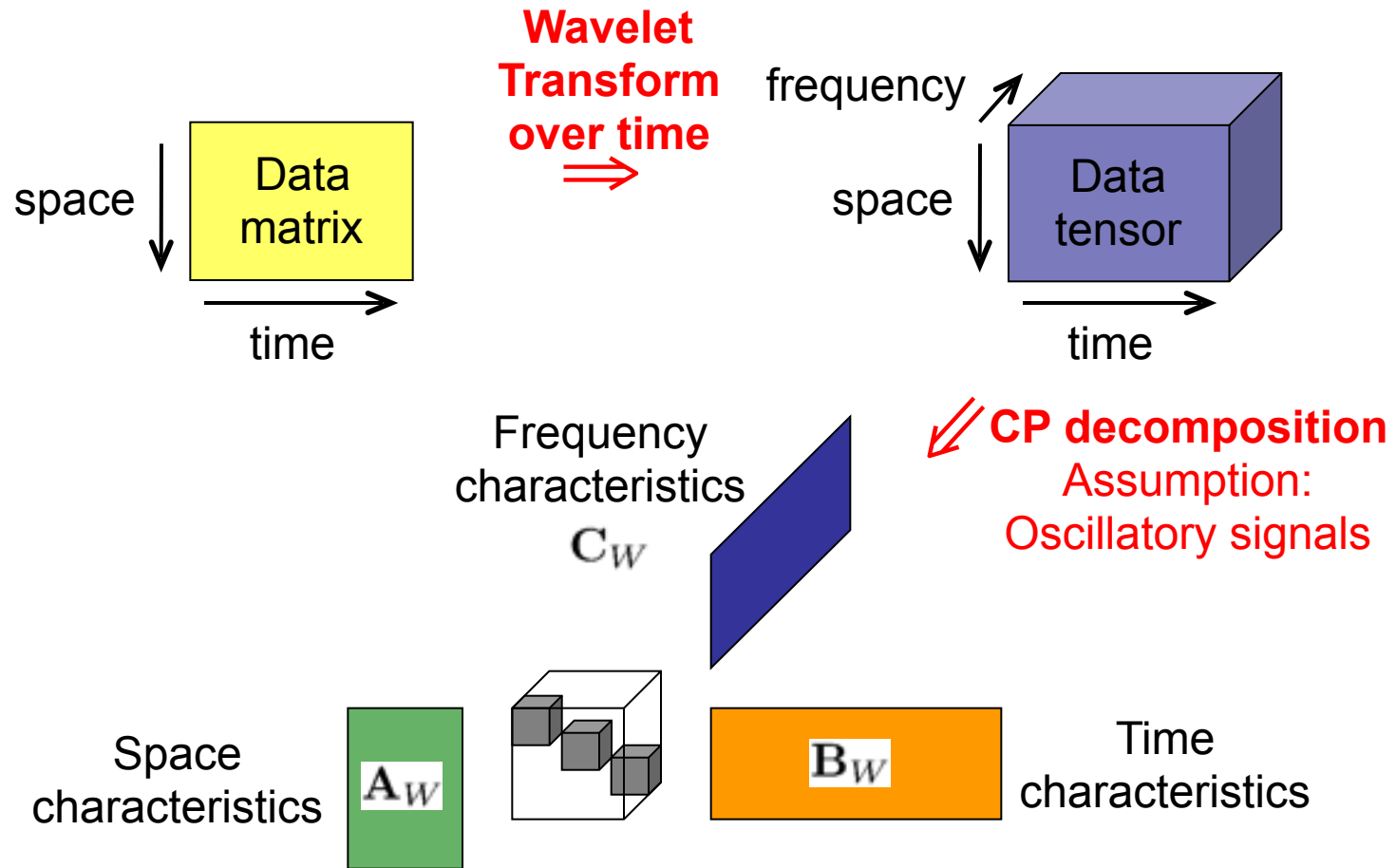
Electric potential data      Wavelet

Exploits temporal changes of the data

# 3.1 Space-Time-Frequency (STF) analysis



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$$W(\mathbf{r}, t, f) \approx \sum_{p=1}^R \mathbf{a}_W(\mathbf{r}; p) \cdot \mathbf{b}_W(t; p) \cdot \mathbf{c}_W(f; p)$$

## 3.2 Space-Time-Wave-Vector (STWV) analysis



Evaluates spatial changes of the data within a spherical window

## 3.2 Space-Time-Wave-Vector (STWV) analysis

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$$F(\mathbf{r}, t, \mathbf{k}) = \int_{-\infty}^{\infty} w(\mathbf{r}' - \mathbf{r}) \cdot x(\mathbf{r}', t) e^{j\mathbf{k}^T \mathbf{r}'} d\mathbf{r}'$$

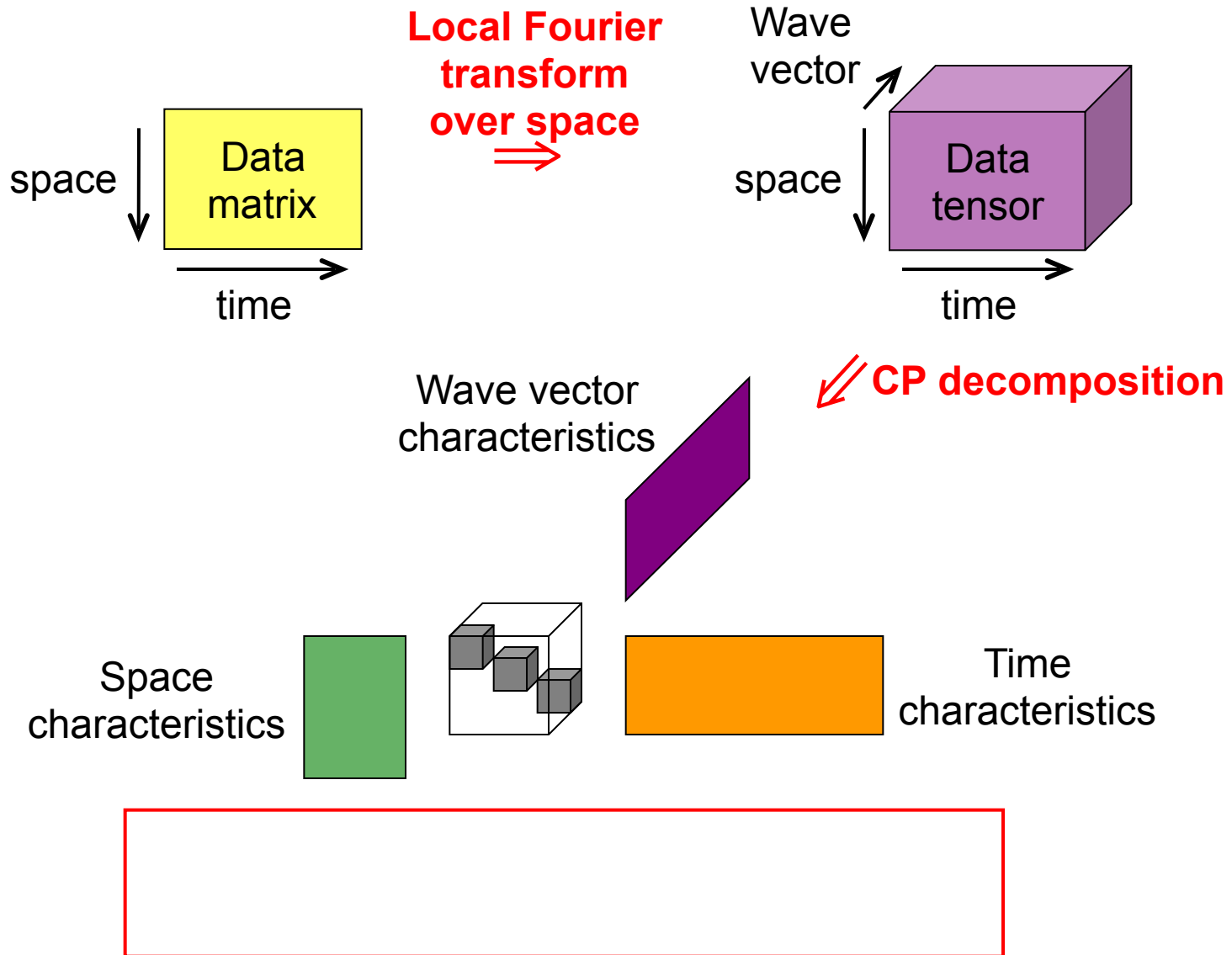
3D window function

Electric potential data

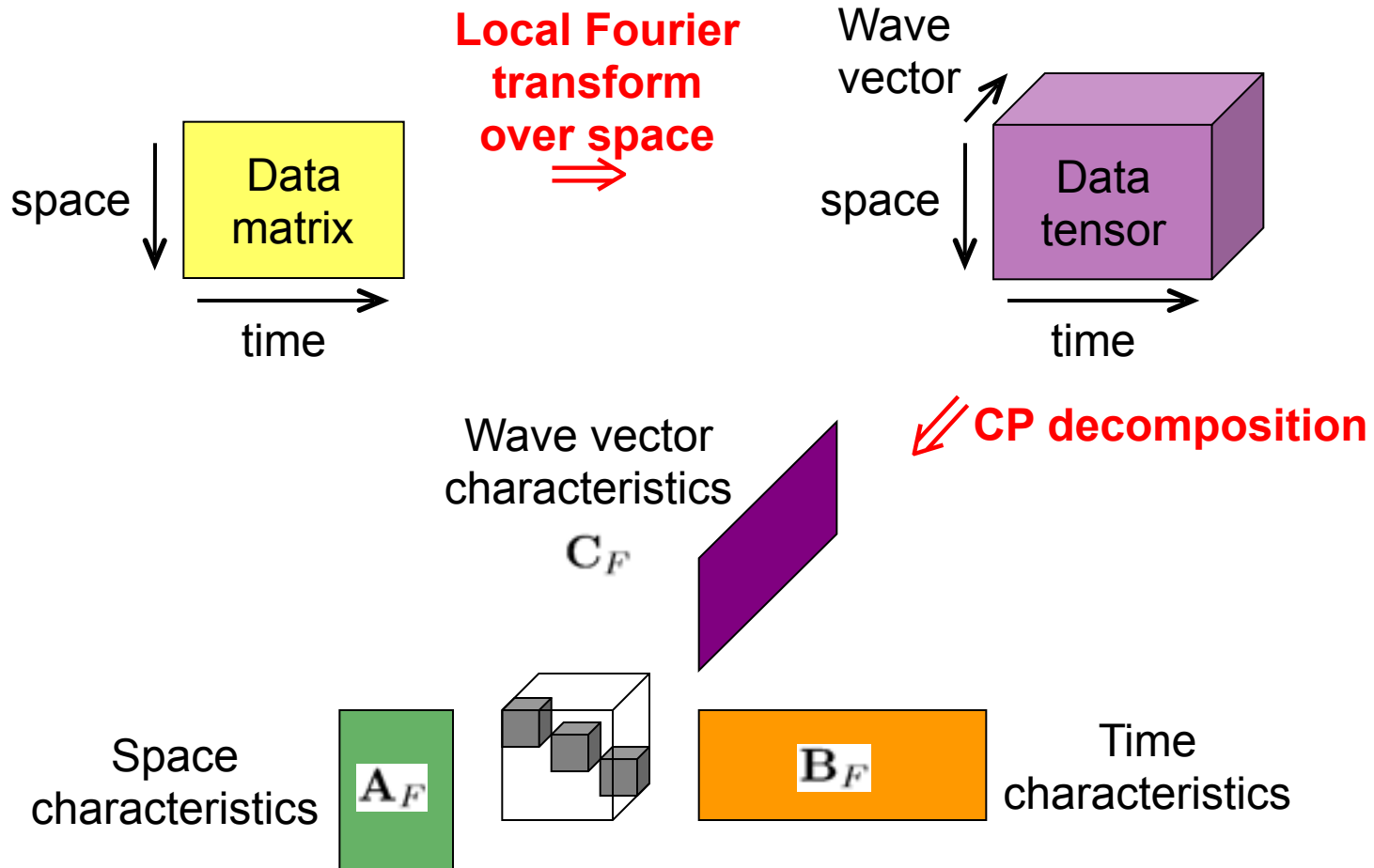
Evaluates spatial changes of the data within a spherical window



# 3.2 Space-Time-Wave-Vector (STWV) analysis



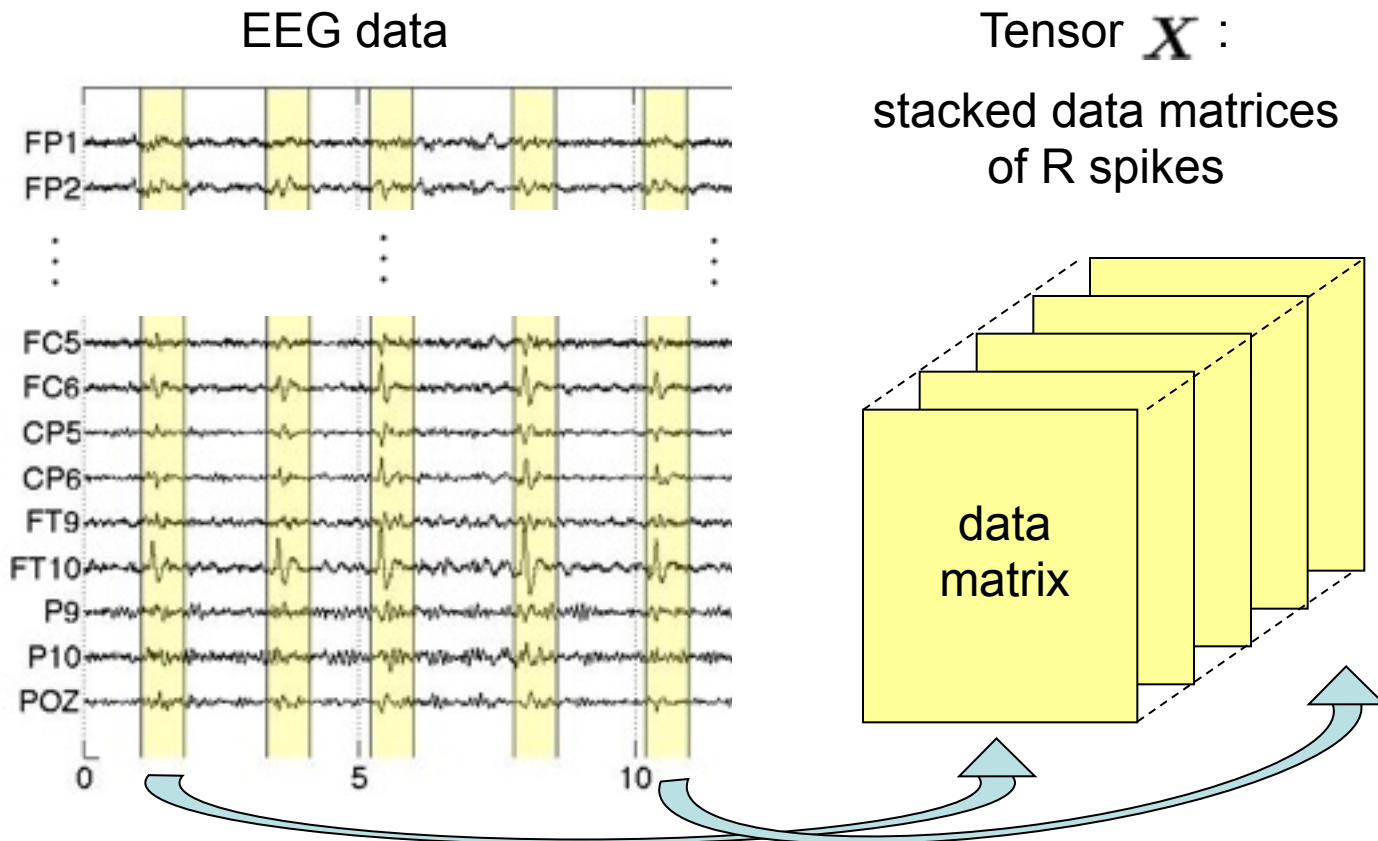
# 3.2 Space-Time-Wave-Vector (STWV) analysis



$$F(\mathbf{r}, t, \mathbf{k}) \approx \sum_{p=1}^R \mathbf{a}_F(\mathbf{r}; p) \cdot \mathbf{b}_F(t; p) \cdot \mathbf{c}_F(\mathbf{k}; p)$$

### 3.3 Construction of a space-time-spike tensor

- Stack EEG data of interictal epileptic spike-like signals observed at different time instants along the third dimension of the tensor [4]



[4] Deburchgraeve et al. 2009 , “Neonatal seizure localization using Parafac decomposition,” Clinical Neurophysiology

# 3.3 CP model of a space-time-spike tensor

□ CP model:

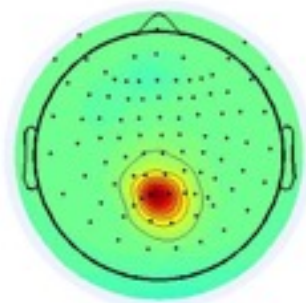
$$X \approx \sum_{p=1}^P \mathbf{h}_p \circ \mathbf{s}_p \circ \mathbf{c}_p$$

spatial maps

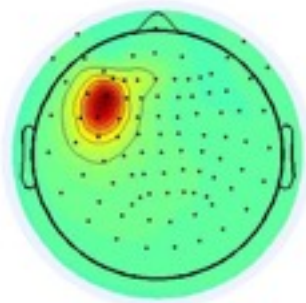
$$\mathbf{H} = [\mathbf{h}_1, \dots, \mathbf{h}_P]$$

e.g.

p=1



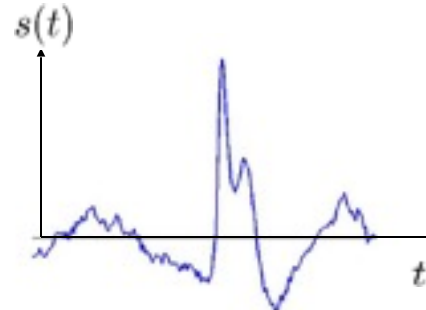
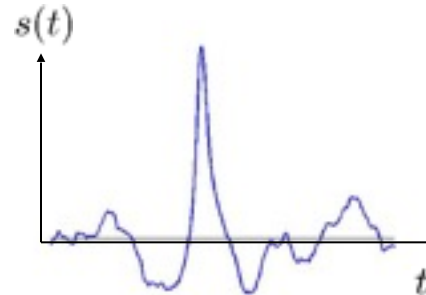
p=2



⇒ spatial

time signals

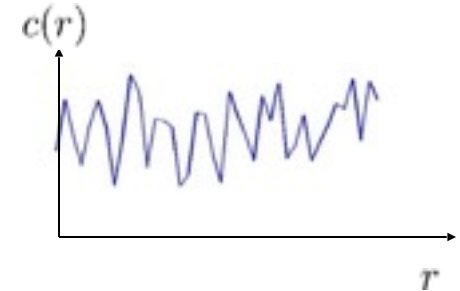
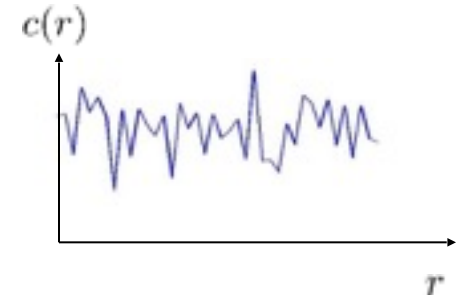
$$\mathbf{S} = [\mathbf{s}_1, \dots, \mathbf{s}_P]$$



and fc

spike amplitudes

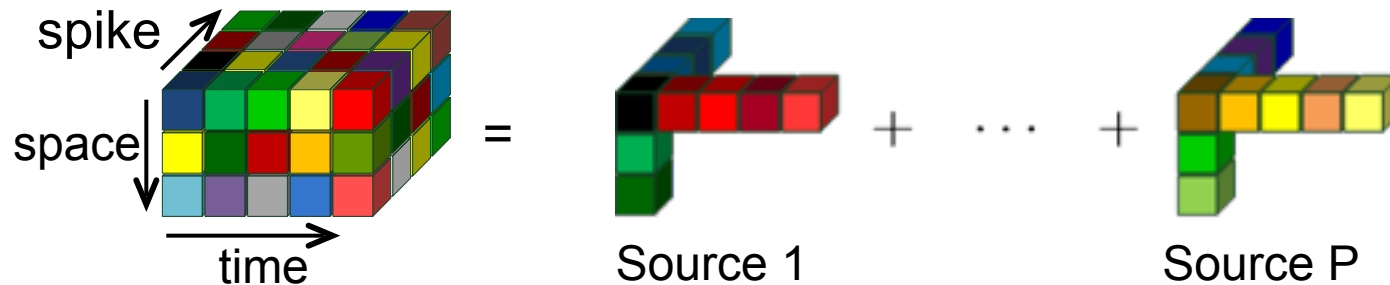
$$\mathbf{C} = [\mathbf{c}_1, \dots, \mathbf{c}_P]$$



## 4.1 Classical two-step tensor-based source localization approach: STS-DA

16

- **First step:** CP decomposition of tensor  $X$  to identify the matrix  $H$



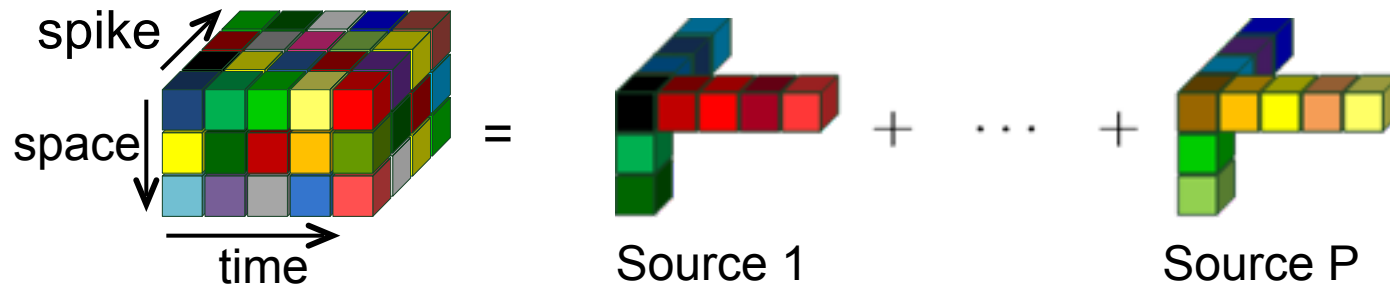
- **Second step:** Separate localization of each distributed source based on
  - the distributed source lead field vector
  - a dictionary of circular-shaped source regions, the “disks”. of varying sizes, which are described by the coefficient vectors  $\mathbf{h}_p = \mathbf{G}\psi_p$
  - a metric

$$M(\mathbf{h}_p, \psi)$$

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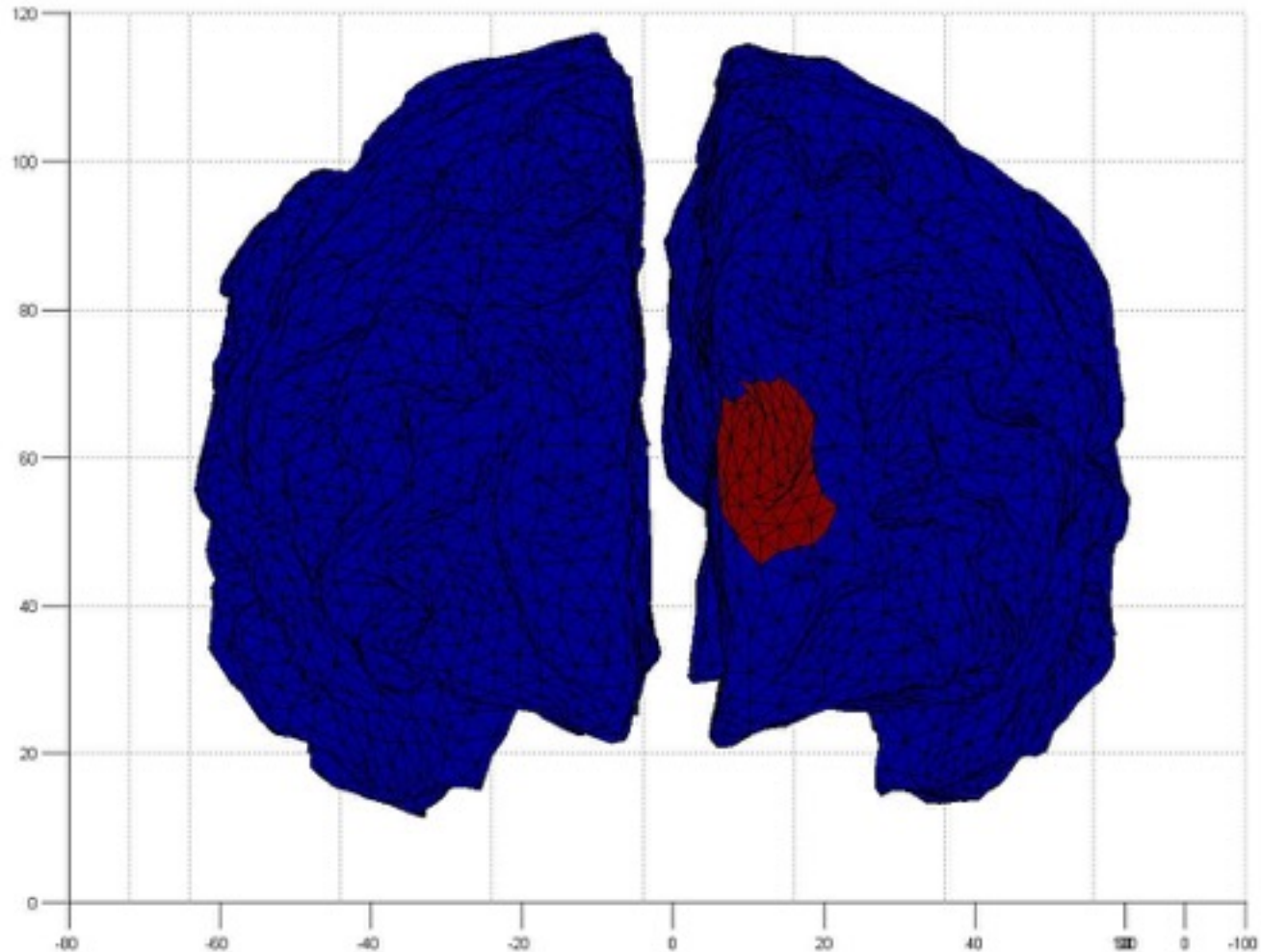


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  - a metric

$$M(\mathbf{h}_p, \psi) = \frac{(\hat{\mathbf{h}}_p^\top \mathbf{G}\psi_p)^2}{\psi_p^\top \mathbf{G}^\top \mathbf{G}\psi_p}$$

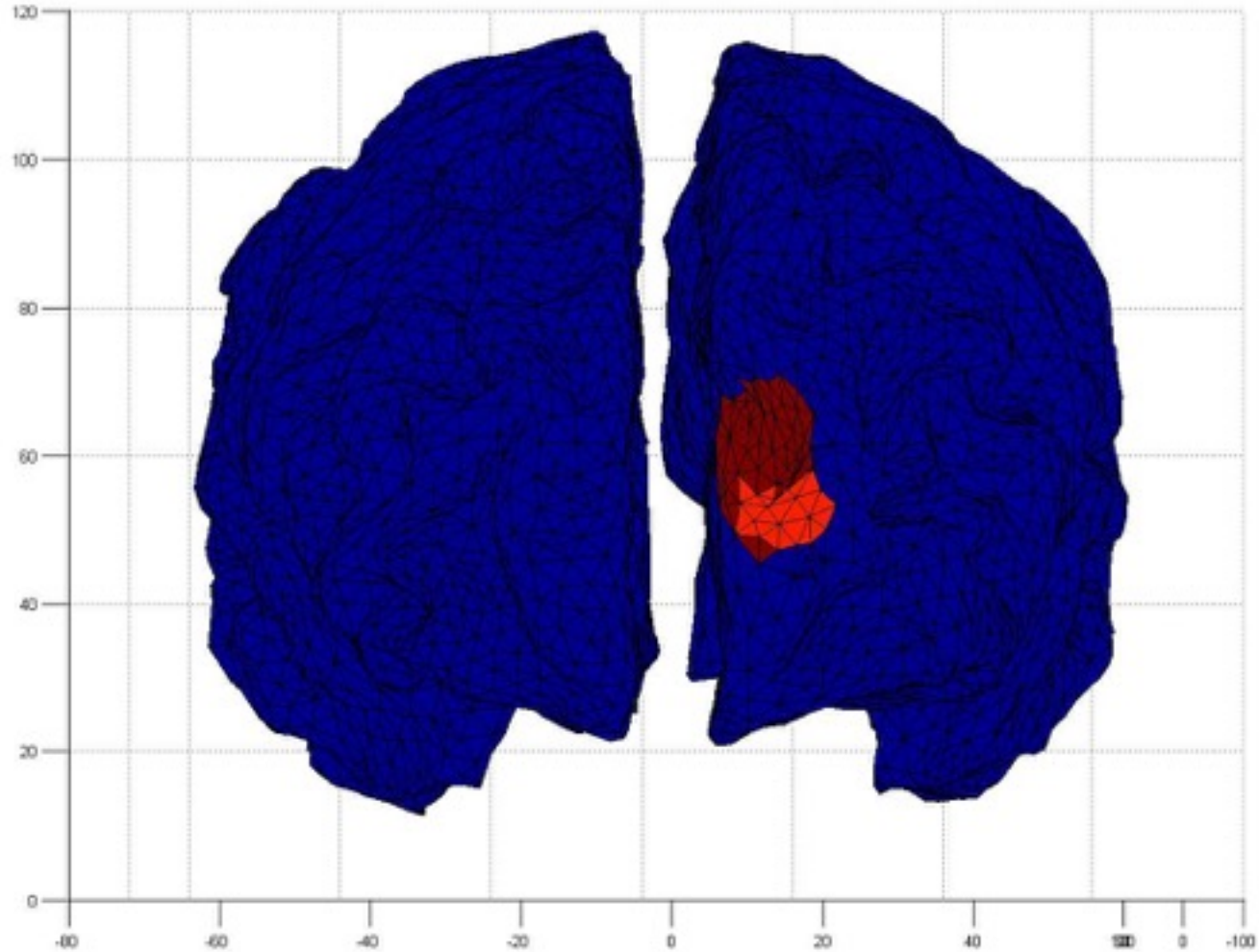
## 4.2 Distributed source localization results: Disk algorithm

17



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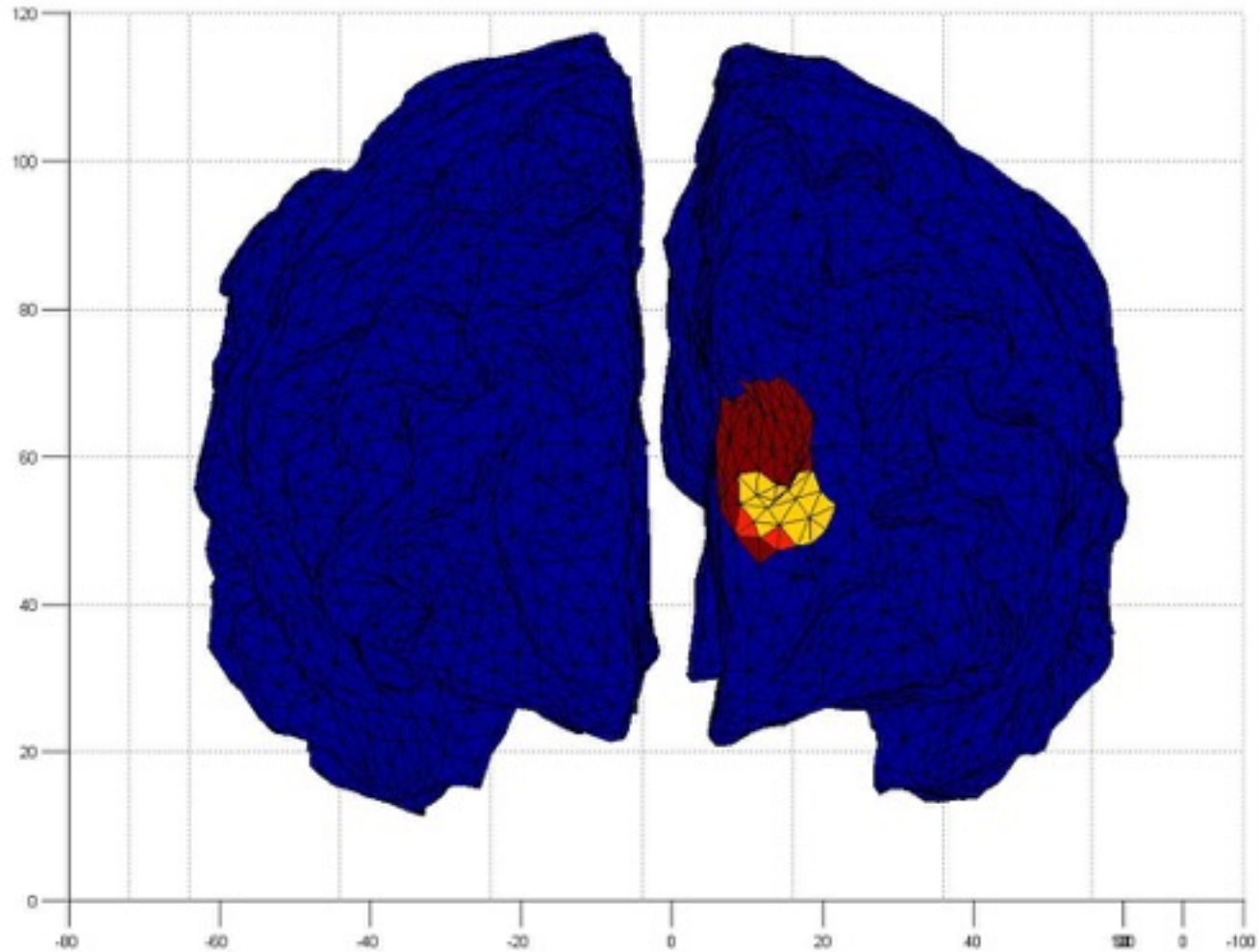
17





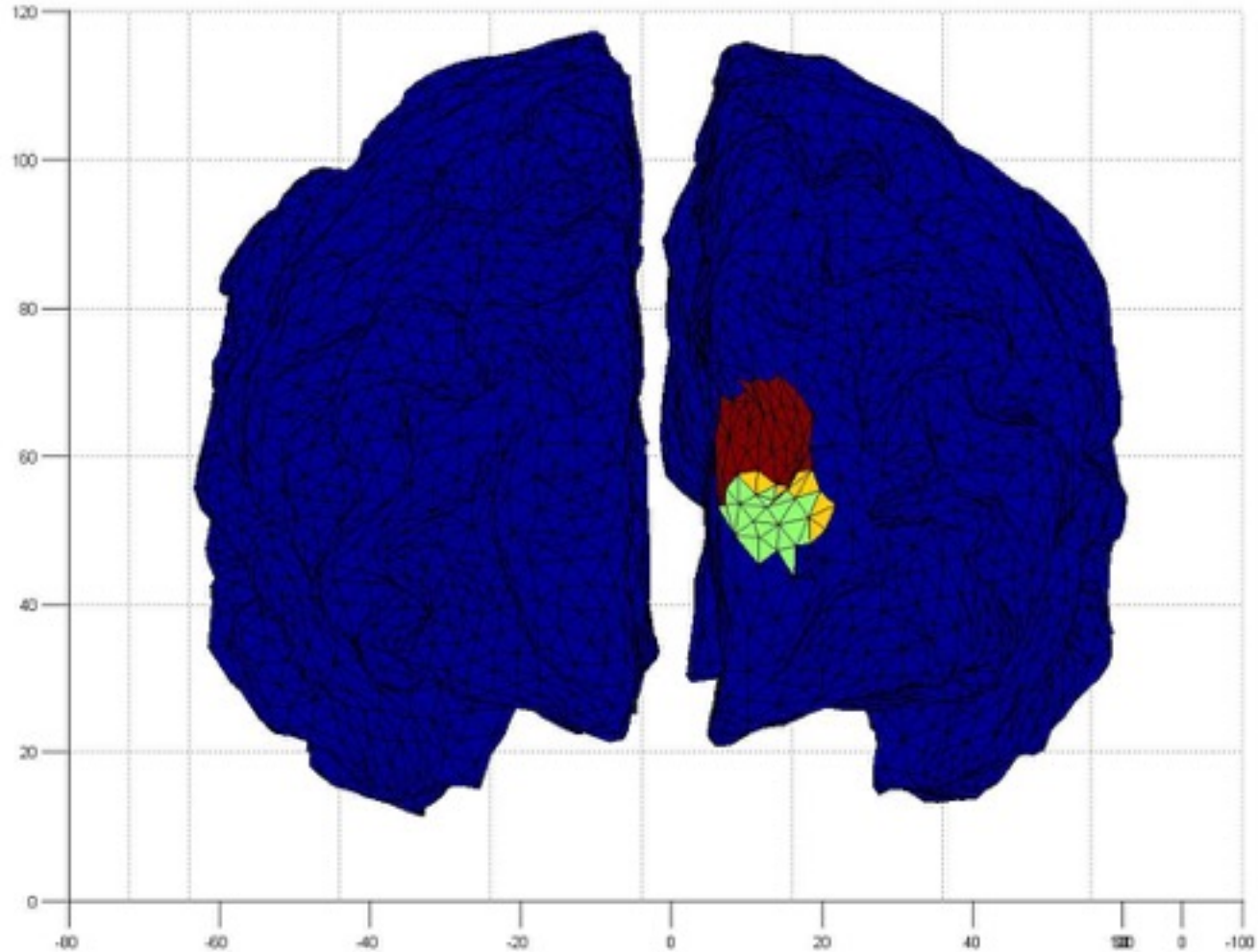
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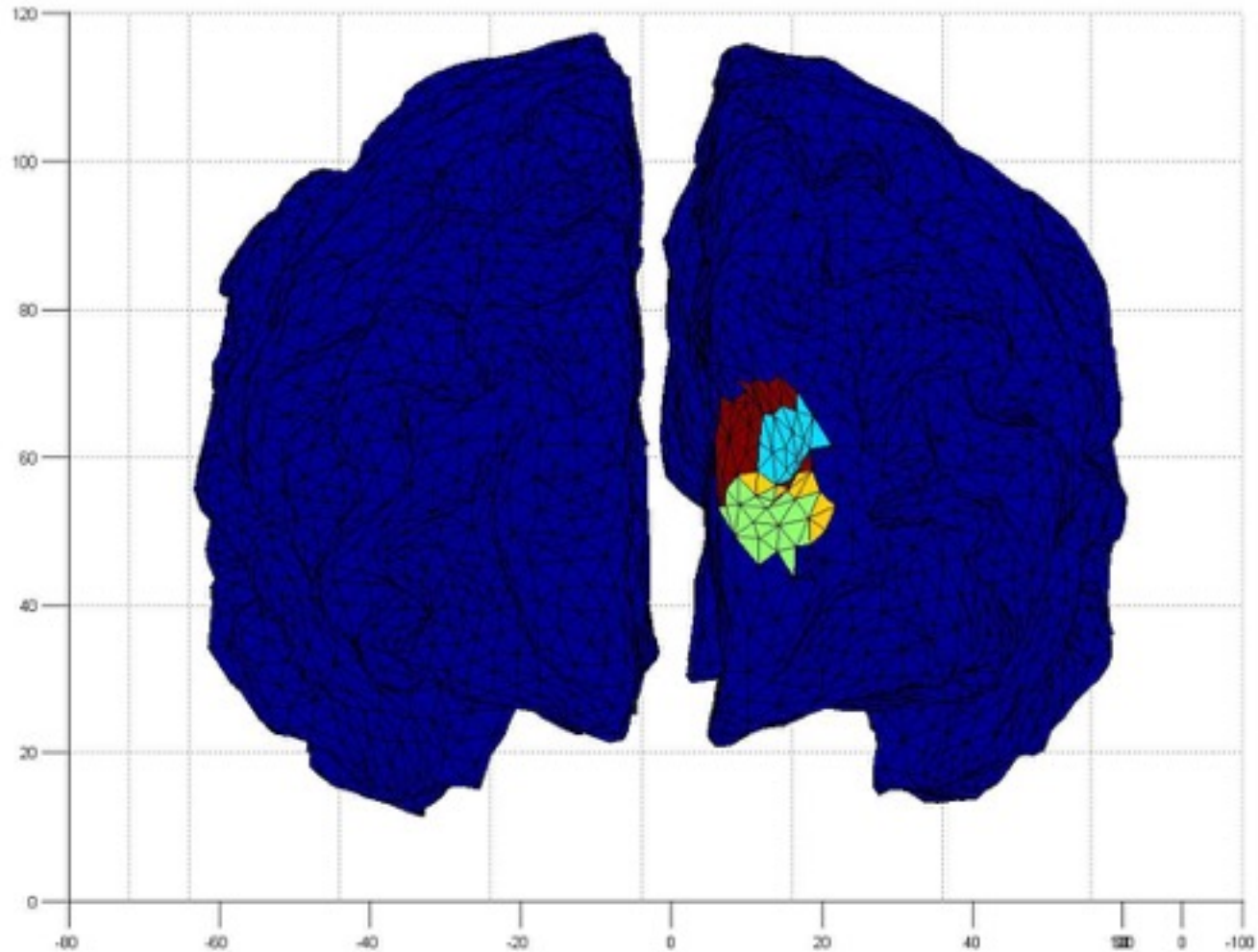
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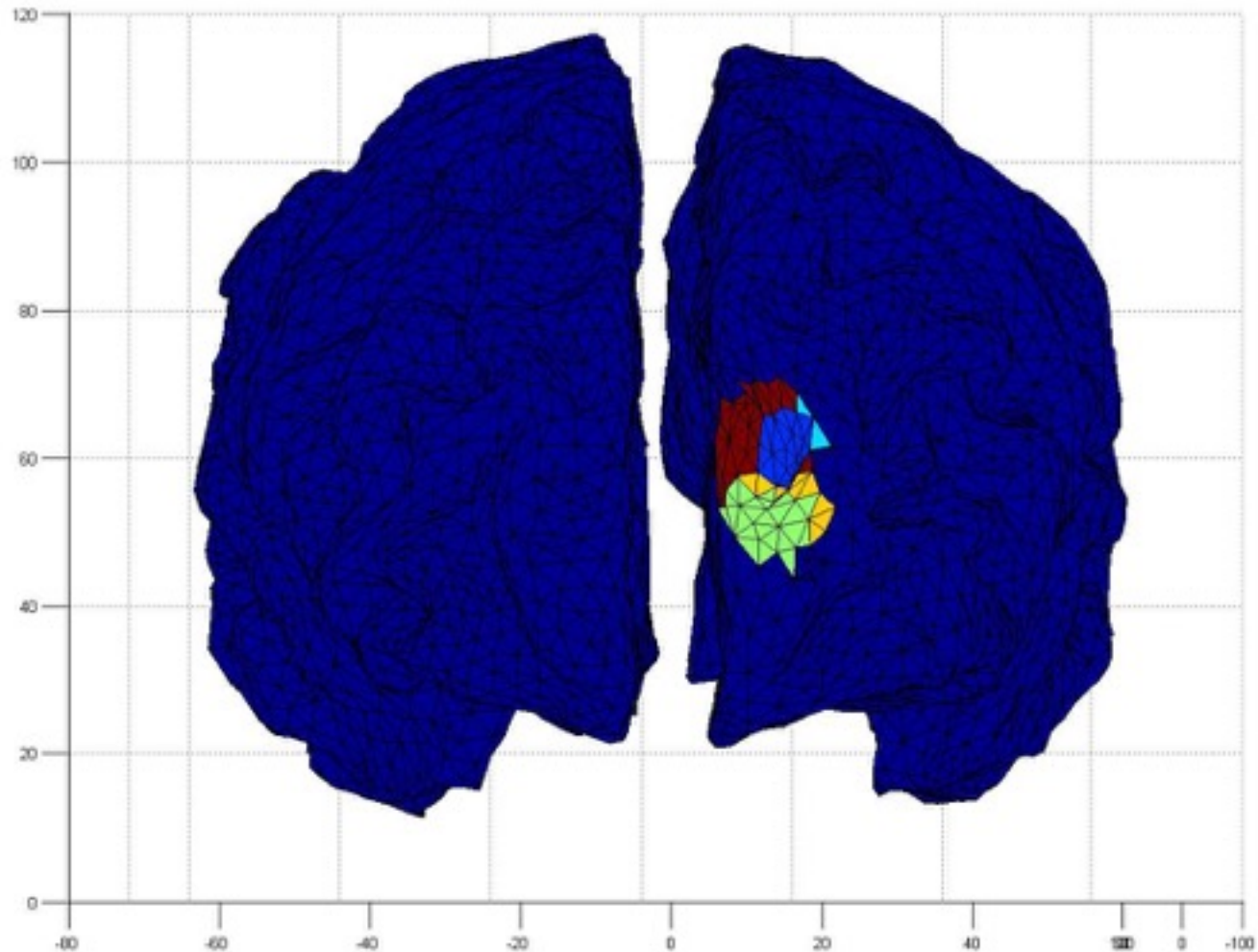
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## 4.3 Proposed single-step approach: STS-SISSY (1)

- **Idea:** Perform tensor decomposition and source localization in a single step
  - Impose structural constraint:  $\mathbf{H} = \mathbf{G}\Psi$  Piecewise-constant spatial distribution
  - Employ fused LASSO regularization:  $\lambda(\|\mathbf{T}\Psi\|_1 + \alpha\|\Psi\|_1)$

gradient operator

$\lambda, \alpha$  – regularization parameters

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- Constrained tensor decomposition based on ALS algorithm:

$$\min_{\mathbf{H}, \Psi} \|\mathbf{X}^{(1)} - \mathbf{H}(\mathbf{C} \odot \mathbf{S})^T\|_F^2 + \lambda(\|\mathbf{T}\Psi\|_1 + \alpha\|\Psi\|_1)$$

$$\text{s. t. } \mathbf{H} = \mathbf{G}\Psi$$

$\mathbf{X}^{(i)}$ : unfolding  $\mathbf{X}$  through its  $i$ -th direction

$$\min_{\mathbf{S}} \|\mathbf{X}^{(2)} - \mathbf{S}(\mathbf{C} \odot \mathbf{H})^T\|_F^2$$

$$\min_{\mathbf{C}} \|\mathbf{X}^{(3)} - \mathbf{C}(\mathbf{S} \odot \mathbf{H})^T\|_F^2$$

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$$\min_{\mathbf{S}} \|\mathbf{X}^{(2)} - \mathbf{S}(\mathbf{C} \odot \mathbf{H})^T\|_F^2 \quad \Rightarrow \quad \mathbf{S} = \mathbf{X}^{(2)} ((\mathbf{C} \odot \mathbf{H})^T)^+$$

$$\min_{\mathbf{C}} \|\mathbf{X}^{(3)} - \mathbf{C}(\mathbf{S} \odot \mathbf{H})^T\|_F^2 \quad \Rightarrow \quad \mathbf{C} = \mathbf{X}^{(3)} ((\mathbf{S} \odot \mathbf{H})^T)^+$$



## 4.4 Proposed single-step approach: STS-SISSY (2)

- Reformulation of the constrained optimization problem:

$$\min_{\mathbf{H}, \mathbf{Y}, \mathbf{Z}} \|\mathbf{X}^{(1)} - \mathbf{H}(\mathbf{C} \odot \mathbf{S})^T\|_F^2 + \lambda(\|\mathbf{Y}\|_1 + \alpha\|\mathbf{Z}\|_1)$$

$$\text{s. t. } \mathbf{H} = \mathbf{G}\Psi, \mathbf{Y} = \mathbf{T}\Psi, \mathbf{Z} = \Psi$$

- Solution using ADMM with update equations:

$$\mathbf{H} = (\mathbf{X}^{(1)}(\mathbf{C} \odot \mathbf{S}) + \rho\mathbf{G}\Psi + \mathbf{V})((\mathbf{C} \odot \mathbf{S})^T(\mathbf{C} \odot \mathbf{S}) + \rho\mathbf{I}_P)^{-1}$$

$$\Psi = (\rho\mathbf{T}^T\mathbf{T} + \rho\mathbf{I}_D + \rho\mathbf{G}^T\mathbf{G})^{-1}\Phi$$

$$\text{with } \Phi = \rho(\mathbf{T}^T\mathbf{Y} + \mathbf{Z} + \mathbf{G}^T(\mathbf{H} - \mathbf{V})) - \mathbf{T}^T\mathbf{U} - \mathbf{W}$$

- Latent variables:

$$\mathbf{Y} = \text{prox}_{\|\cdot\|_1, \frac{\lambda}{\rho}}(\mathbf{T}\Psi + \mathbf{U}/\rho)$$

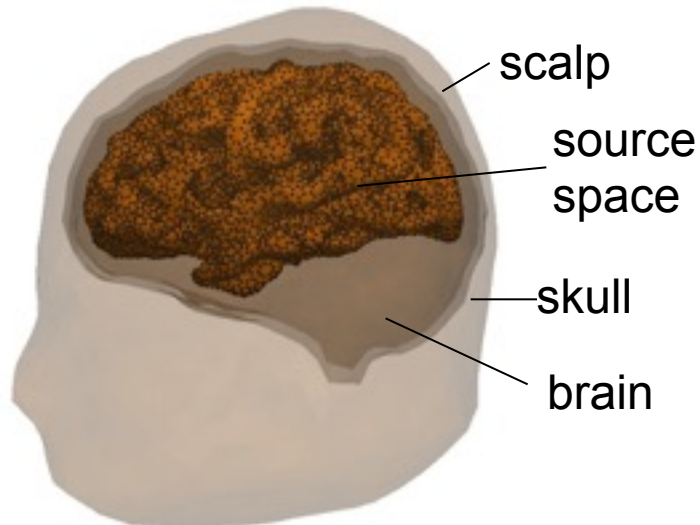
$$\mathbf{Z} = \text{prox}_{\|\cdot\|_1, \frac{\lambda\alpha}{\rho}}(\Psi + \mathbf{W}/\rho)$$

- Lagrangian multipliers:

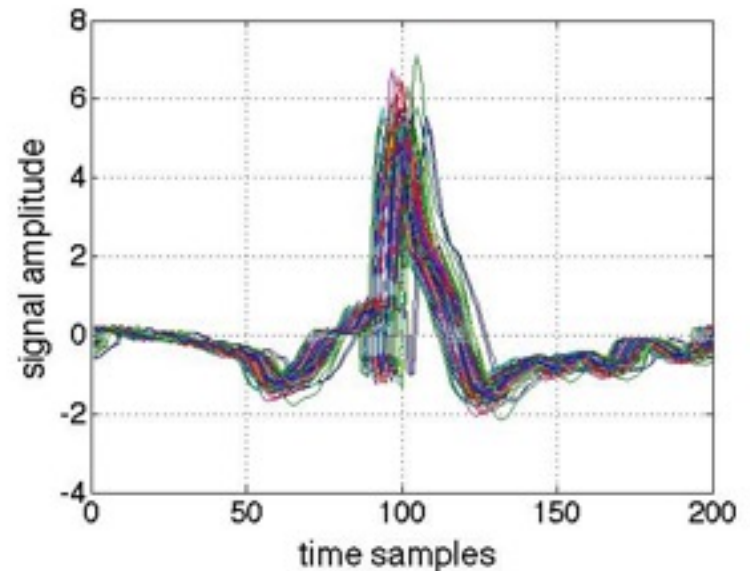
$$\Delta\mathbf{U} = \rho(\mathbf{T}\Psi - \mathbf{Y}); \Delta\mathbf{V} = \rho(\mathbf{G}\Psi - \mathbf{H}); \Delta\mathbf{W} = \rho(\Psi - \mathbf{Z})$$

# 5. Simulation setup

- Realistic head model



- SEEG signals for patch dipoles



- Extended sources (patches) composed of adjacent grid dipoles
- Highly correlated interictal epileptic spike activities within a patch
- Two sources:
  - One source composed of two patches with delayed spike-like signals
  - One source composed of one patch with spike-like signals of slightly different morphology than for the first source
- 91 sensors, 50 realizations of spikes with different amplitudes

# 5.1 Evaluation criterion and performance results <sup>21</sup>

- **Evaluation criterion: dipole localization error (DLE)**

$$\text{DLE} = \frac{1}{2} \left( \frac{1}{\#\mathcal{I}} \sum_{k \in \mathcal{I}} \min_{\ell \in \hat{\mathcal{I}}} \|\mathbf{r}_k - \mathbf{r}_\ell\| + \frac{1}{\#\hat{\mathcal{I}}} \sum_{\ell \in \hat{\mathcal{I}}} \min_{k \in \mathcal{I}} \|\mathbf{r}_k - \mathbf{r}_\ell\| \right)$$

$\mathcal{I}$  – Set containing the indices of active grid dipoles

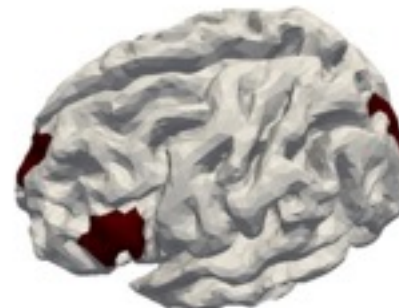
$\hat{\mathcal{I}}$  – Set containing the indices of estimated active grid dipoles

$\mathbf{r}_k$  – Position of the k-th grid dipole

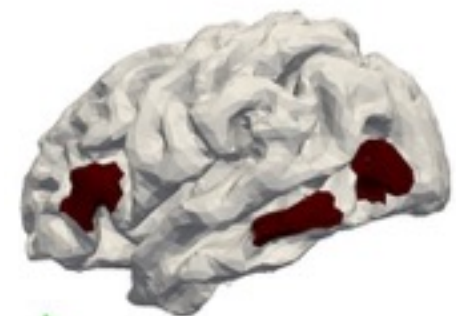
- **Performance results for two scenarios:**

scenario	Single-step STS-SISSY	Two-step STS-DA
1	1.32	18.23
2	1.37	7.29

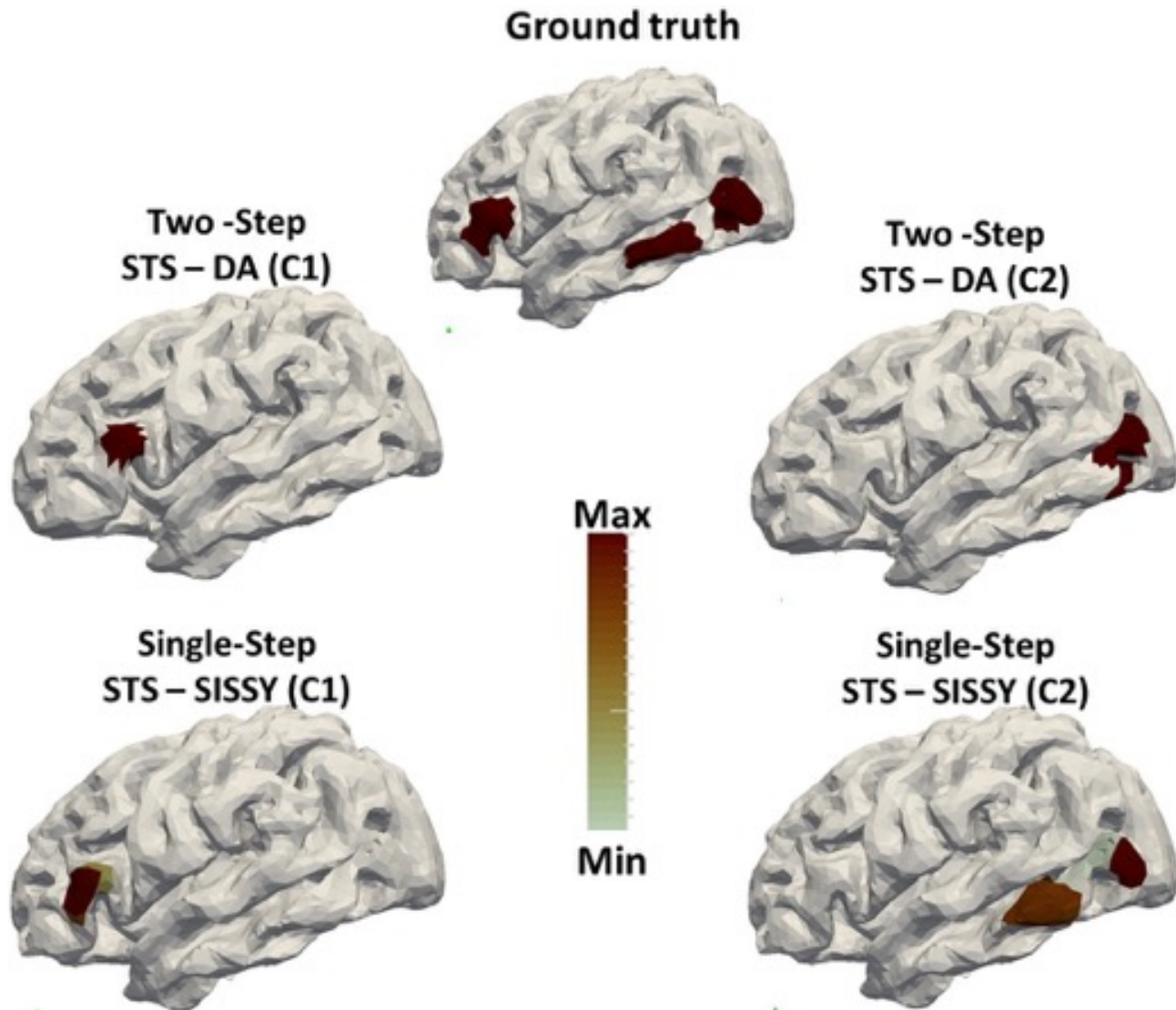
Scenario 1



Scenario 2



## 5.2 Illustration of simulation results



- ❑ EEG sources can be separated and localized in a single step by the proposed constrained tensor decomposition approach
- ❑ The proposed algorithm makes use of the ALS and ADMM optimization strategies
- ❑ Realistic simulations in the context of drug-resistant epilepsy have shown that the proposed single-step method outperforms a previously developed two-step tensor-based source localization approach

- [1] F. Miwakeichi, E. Martinez-Montes, P. A. Valdes-Sosa, N. Nishiyama, H. Mizuhara, and Y. Yamaguchi, “Decomposing EEG data into space-time-frequency components using parallel factor analysis,” *NeuroImage*, 2004.
- [2] H. Becker, P. Comon, L. Albera, M. Haardt, and I. Merlet, “Multi-way space-time-wave-vector analysis for EEG source separation,” *Signal Processing*, 2012
- [3] M. Morup, L. K. Hansen, C. S. Herrmann, J. Parnas, and S. M. Arnfred, “Parallel factor analysis as an exploratory tool for wavelet transformed event-related EEG,” *NeuroImage*, 2006
- [4] W. Deburchgraeve, P. J. Cherian, M. De Vos, R. M. Swarte, J. H. Blok, G. H. Visser, P. Govaert, and S. Van Huffel, “Neonatal seizure localization using Parafac decomposition,” *Clinical Neurophysiology*, 2009
- [5] M. Weis, D Jannek, T Guenther, P Husar, F. Roemer, M. Haardt, “Temporally resolved multi-way component analysis of dynamic sources in event-related EEG data using PARAFAC2,” *Proc. of EUSIPCO 2010*

- [6] M. Morup, L. K. Hansen, S. M. Arnfred, L.-H. Lim, and K. H. Madsen, "Shift-invariant multilinear decomposition of neuroimaging data," NeuroImage, 2008
- [7] B. Hunyadi, D. Camps, L. Sorber, W. Van Paesschen, M. De Vos, S. Van Huffel, and L. De Lathauwer, "Block term decomposition for modelling epileptic seizures," EURASIP Journal on Advances in Signal Processing, 2014
- [8] H. Becker, L. Albera, P. Comon, M. Haardt, G. Birot, F. Wendling, M. Gavaret, C. G. B'énar, and I. Merlet, "EEG extended source localization: tensor-based vs. conventional methods," NeuroImage, 2014