

# Graph theory to explore resting state brain functional connectivity

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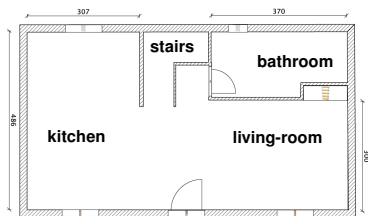
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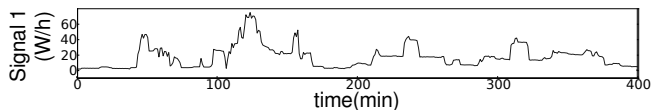
# Multivariate time series structured in a network

*A simple example: recording electric consumption*

A simple sensor recording the overall electricity consumption



Observed univariate time series



$$X(k) \\ 1 \leq k \leq N$$

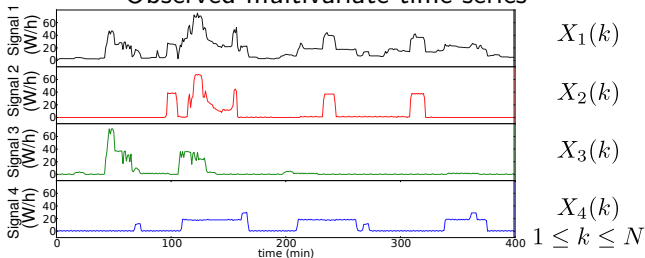
[Harlé et al. IEEE Trans. Sig. Proc. 2016]

# Multivariate time series structured in a network

Multiple sensors in different places of the house

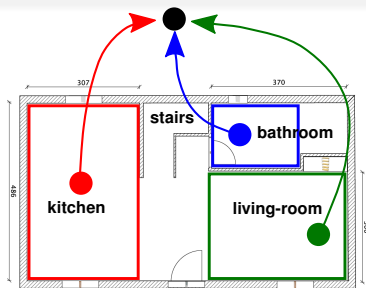


Observed multivariate time series

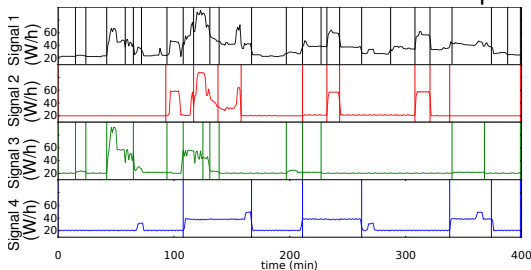


# Multivariate time series structured in a network

Multiple sensors in different places of the house with possible links



Observed multivariate time series with multiple change point detection

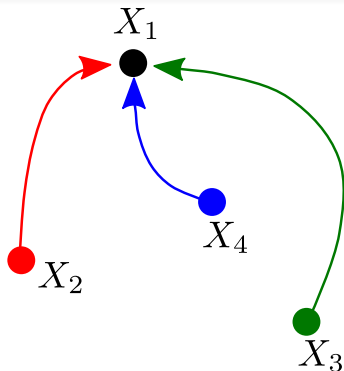


$$\begin{pmatrix} X_1(k) \\ X_2(k) \\ X_3(k) \\ X_4(k) \end{pmatrix} = \mathbf{X}(k) \quad 1 \leq k \leq N$$

[Harlé et al. IEEE Trans. Sig. Proc. 2016]

# Multivariate time series structured in a network

Definition of the network (or graph):

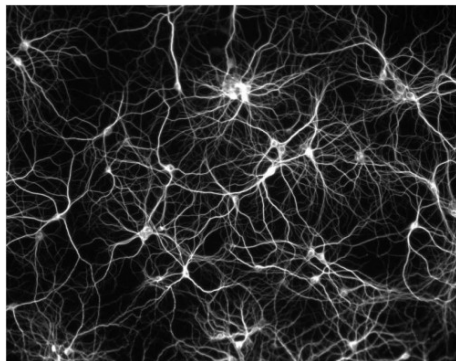


- nodes:  $X_1$ ,  $X_2$ ,  $X_3$  and  $X_4$
- edges:  $X_2 \rightarrow X_1$ ,  $X_3 \rightarrow X_1$ ,  $X_4 \rightarrow X_1$
- adjacency matrix:

$$\begin{bmatrix} 0 & 0 & 0 & 0 \\ 1 & 0 & 0 & 0 \\ 1 & 0 & 0 & 0 \\ 1 & 0 & 0 & 0 \end{bmatrix}$$

[Harlé et al. IEEE Trans. Sig. Proc. 2016]

# The brain as a network



- $10^{11}$  neurons
- Connected via axons and dendrites ( $10^{14}$  connections)
- Transmission of nerve signals (segregated and distributed information)

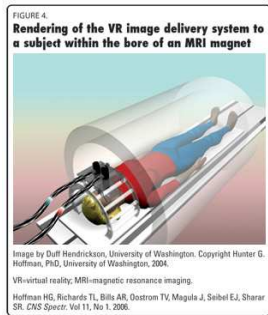
# Exploring the brain using networks analysis

## Functional Magnetic Resonance Imaging – fMRI:

[Ogawa 1990, Kwong 1991]

Measure of the haemodynamic response related to neural activity in the brain.

**BOLD**(Blood-oxygen-level dependent)= MRI contrast of blood deoxyhemoglobin



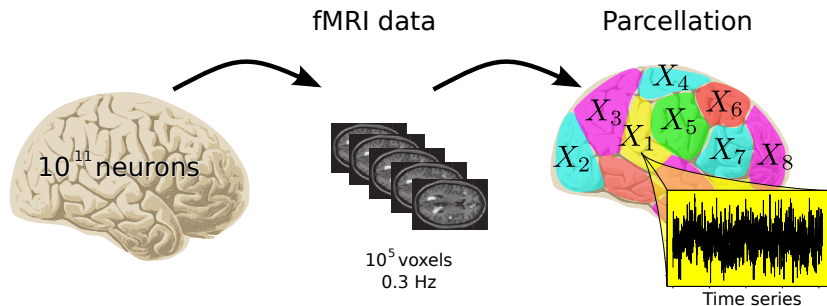
Copyright Hunter G Hoffman.



IRMaGe, GIN, UGA

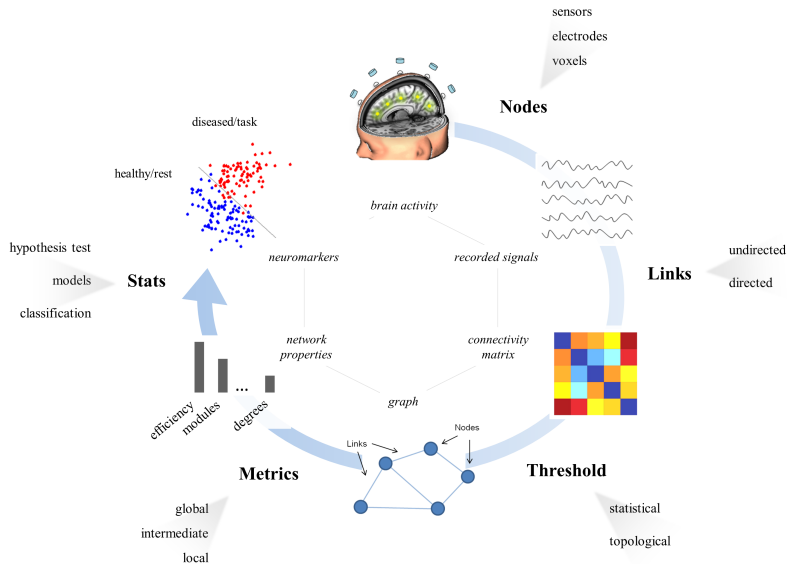
# Exploring the brain using networks analysis

## Hundreds of time series corresponding to brain regions



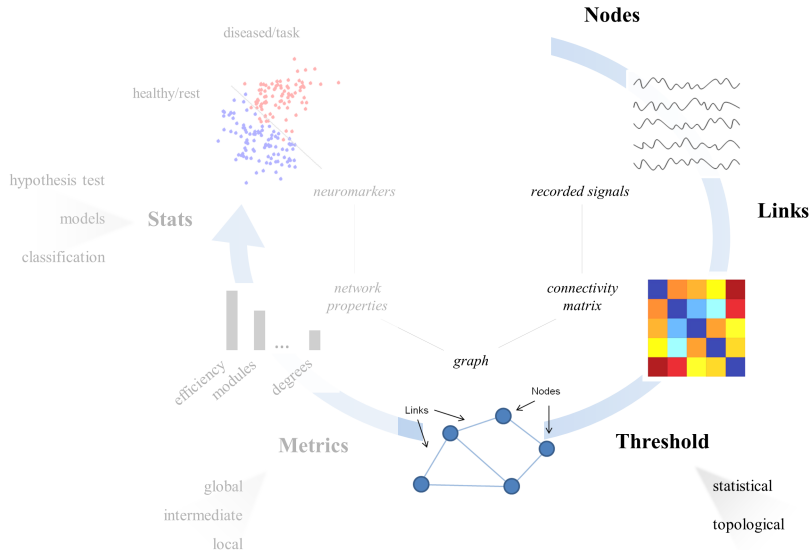


# Exploring the brain using networks analysis

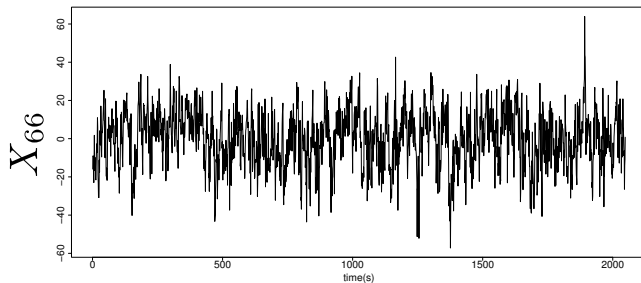
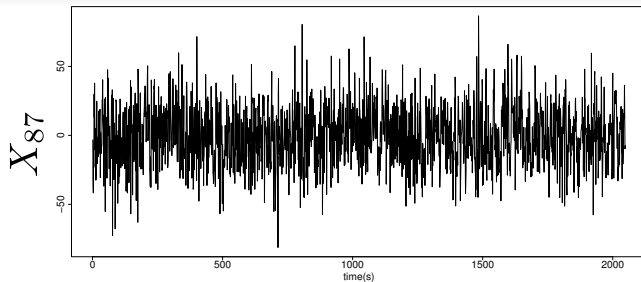


[De Vico Fallani *et al.* Phil. Trans. Roy. B 2014]

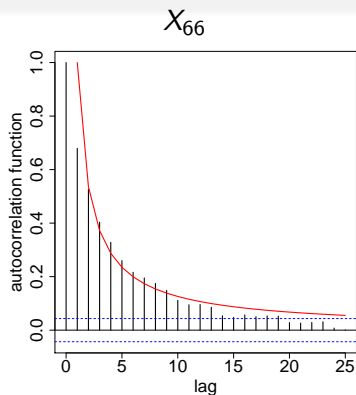
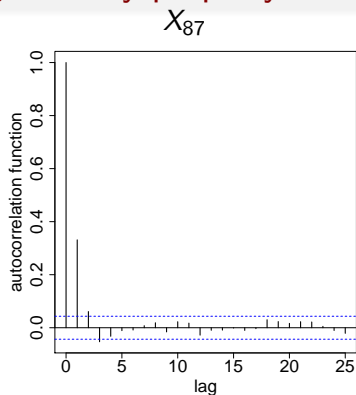
# Part I: Inference of networks



# Long memory property of the brain time series



# Long memory property of the brain time series



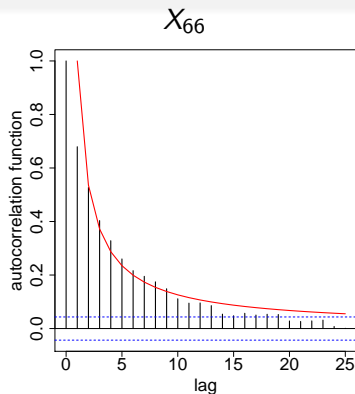
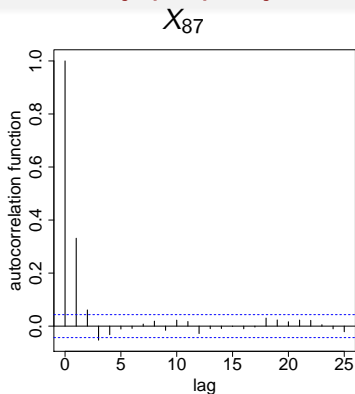
autocorrelations not summable

$$\rho(\lambda) = \text{Corr}(X(t + \lambda), X(t)) \sim \lambda^{2d-1}$$

Note: For an *ARMA* process,

$$|\rho(\lambda)| \leq b|a|^\lambda, \quad 0 < b < \infty, \quad 0 < a < 1$$

# Long memory property of the brain time series



autocorrelations not summable

A simple example,  $X(1), \dots, X(N)$ , random variables,

$$\hat{X} := N^{-1} \sum_{i=1}^N X(i), \quad \mathbb{V}(\hat{X}) = \frac{\sigma^2}{N^2} \sum_{i,j=1}^N \text{Corr}(X(i), X(j))$$

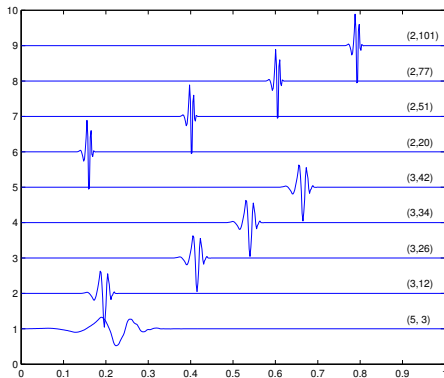
# Wavelets and long memory time series

Let  $(\phi, \psi)$  define a father and a mother wavelets

For any scale  $j \geq 0$  and location  $k \in \mathbb{Z}$  we consider the wavelet coefficient of the signals  $X_\ell(\cdot)$ , for  $\ell = 1, \dots, p$ ,

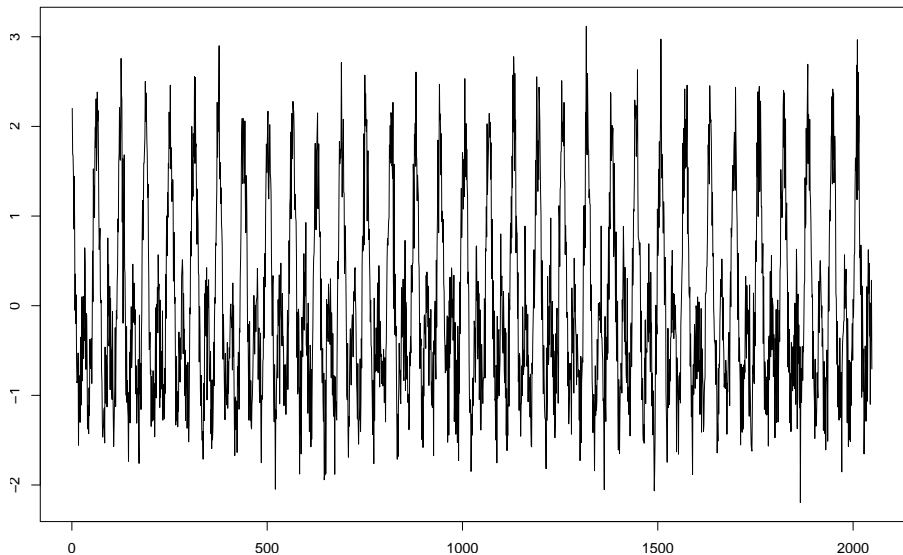
$$W_{j,k}(\ell) \approx \int X_\ell(t) \psi_{j,k}(t) dt$$

An example of  $\psi$ , Daubechies 8

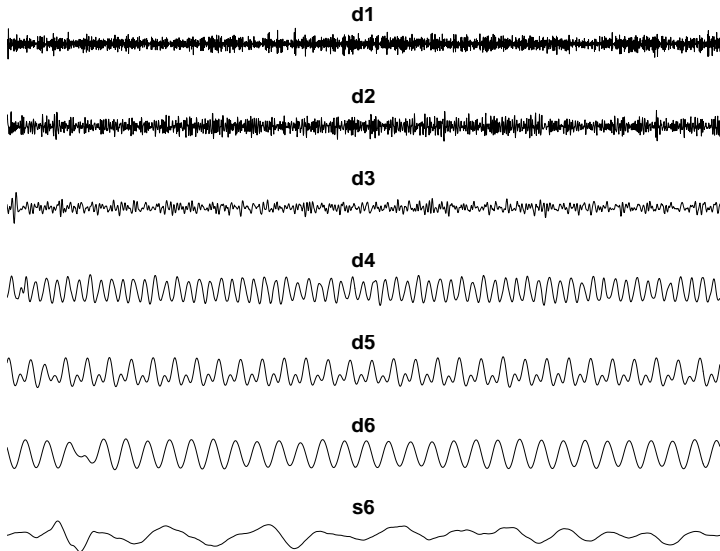


# An example of wavelet decomposition

Example with a signal  $X(t) = \cos(t/5) + \cos(t/10) + \mathcal{N}(0, 0.4)$ :



$$X(t) = \cos(t/5) + \cos(t/10) + \mathcal{N}(0, 0.4)$$





# Wavelets and correlation

$\mathbf{X} = \{\mathbf{X}(k), k \in \mathbb{Z}\}$  long memory process,  $1 \leq \ell, m \leq p$ ,

Wavelet variance

$$\sigma_{\ell}^2(j) = \mathbb{V}(W_{j,k}(\ell))$$
$$\hat{\sigma}^2(j) := \frac{1}{n_j} \sum_{k=0}^{n_j} W_{j,k}^2$$

Wavelet covariance

$$\theta_{\ell,m}(j) = \text{Cov}(W_{j,k}(\ell), W_{j,k}(m))$$
$$\hat{\theta}_{\ell,m}(j) := \frac{1}{n_j} \sum_{k=0}^{n_j} (W_{j,k}(\ell)W_{j,k}(m))$$

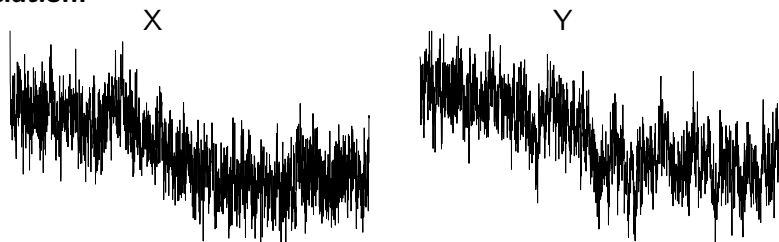
[Percival *et al.* 2000]  
[Whitcher *et al.* 2000]

Wavelet correlation

$$\rho_{\ell,m}(j) = \frac{\theta_{\ell,m}(j)}{\sigma_{\ell}(j)\sigma_m(j)}$$

# Wavelets and correlation

Example of the non consistency of the classical estimator of correlation:



$$\text{Correlation}(X,Y) = 0.597$$

Wavelet correlation :

Scale 1	Scale 2	Scale 3	Scale 4	Scale 5	Scale 6	Remainder
0.059	0.053	0.029	0.08	0.115	0.041	1

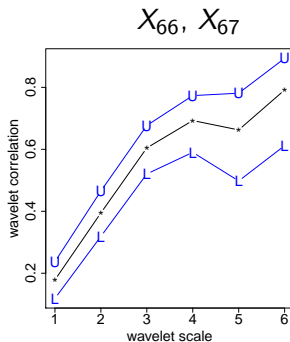
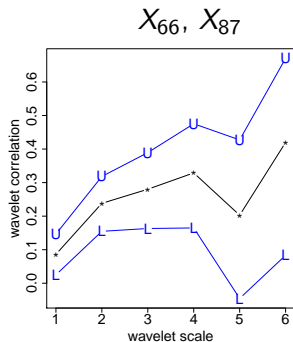
# Wavelets and correlation

## Proposition

$\mathbf{X} = \{\mathbf{X}(k), k \in \mathbb{Z}\}$  long memory process,  $\hat{\rho}_{\ell,m}(j) := \hat{\theta}_{\ell,m} / (\hat{\sigma}_{\ell}(j)\hat{\sigma}_m(j))$

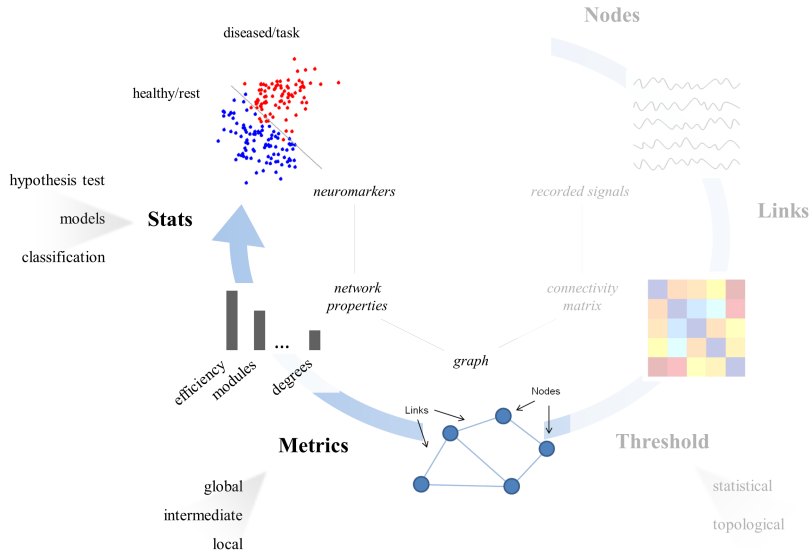
$$\sqrt{(n_j - 3)(z(\hat{\rho}_{\ell,m}(j)) - z(\rho_{\ell,m}(j)))} \xrightarrow{\mathcal{L}} \mathcal{N}(0, 1)$$

where  $z$  in the Fisher transform.



[Achard and Gannaz J. Time Series Analysis 2015] [Achard et al. J. Neurosci. 2006] [Whitcher et al. 2000]

# Part II: Comparison of networks, assessing reliability



# Construction of the adjacency matrices

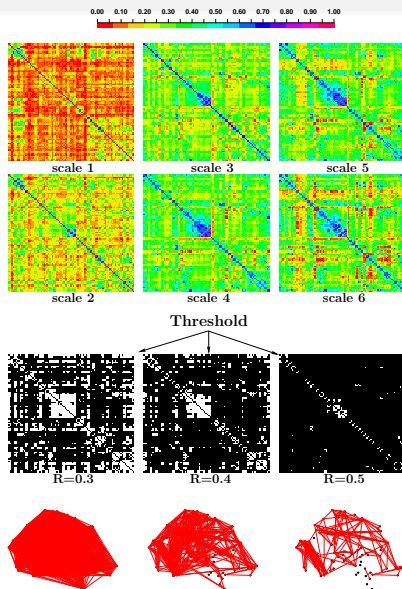
→ pair-wise inter-regional correlations

- Wavelets MODWT
- Connectivity = Correlation

→ adjacency matrix  
Threshold ?

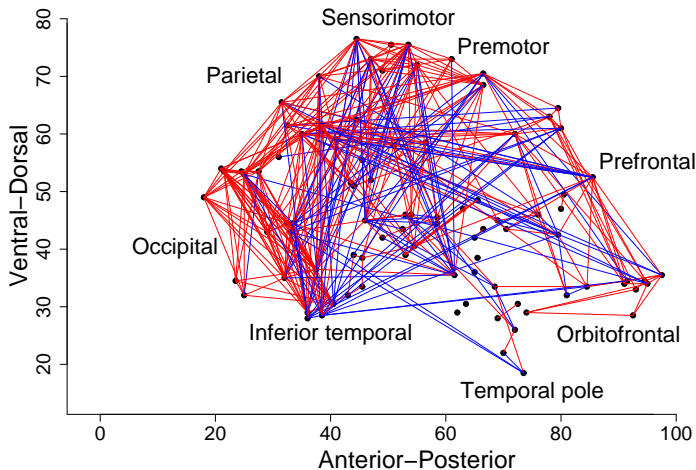
→ Undirected graphs :  
small-world properties

[Achard *et al.* J. Neurosci. 2006]



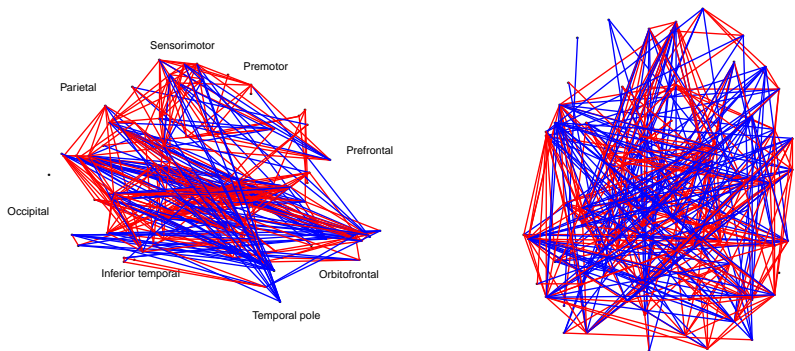
# Individual graphs: representation of networks for a given threshold

90 regions in the brain – 40 minutes scanning – 400 mostly connected pairs



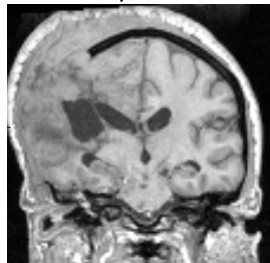
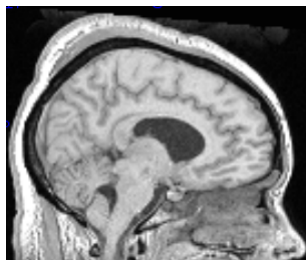
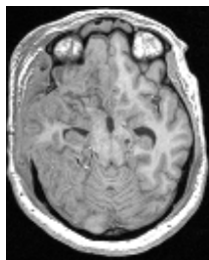
# An example with fMRI data

90 regions in the brain – 5 minutes scanning – 400 mostly connected pairs

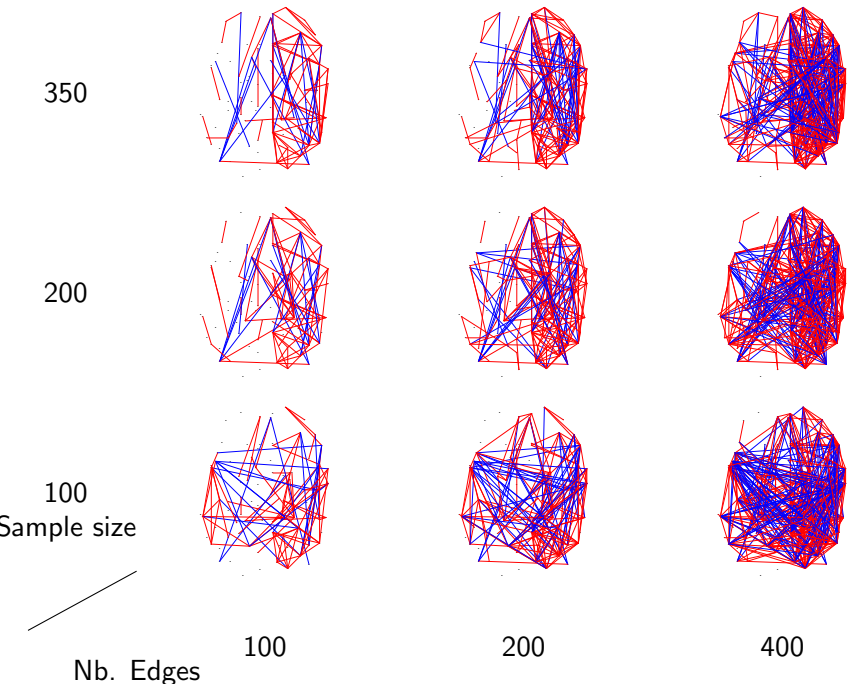


## An example with fMRI data

An example using a patient with craniectomy on the left part of the brain.







# Construction of the adjacency matrices

Hypothesis tests: for all  $i, j, 1 \leq i, j \leq p, i \neq j$

$$\mathcal{H}_0 : \rho_{i,j} = 0 \quad \mathcal{H}_1 : \rho_{i,j} \neq 0$$

Problems :

- Multiple hypotheses tests : 4005 tests
  - Need to compare graphs with same number of edges
  - Maximise interesting properties
- The tests are dependent, classical approaches are not working

[Achard *et al.* J. Neurosci. 2006]  
[Hero *et al.* 2013]  
[Drton *et al.* 2004]

## Multiple hypotheses tests

Number of errors committed when testing 4005 null hypothesis

$n_0$  = number of true null hypotheses

	Not rejected	Rejected	Total
True null hypotheses	<b>U</b>	<b>V</b>	$n_0$
Non-true null hypotheses	<b>T</b>	<b>S</b>	$4005 - n_0$
	$4005 - \mathbf{W}$	<b>W</b>	4005

- $PCER = E(\mathbf{V}/4005) < \alpha$  if each tests control at level  $\alpha$ .  
→ do not take into account the multiple test.
- $FWER = P(\mathbf{V} \geq 1) < \alpha$  if each tests control at level  $\alpha/4005$ .  
→ Problem when the number of hypotheses is large, too conservative.
- $FDR = P(\mathbf{W} > 0)E(\mathbf{V}/\mathbf{W}|\mathbf{W} > 0)$ , i.e. control of the proportion of rejected null hypotheses which are erroneously rejected.  
→ less stringent, and a gain in power.

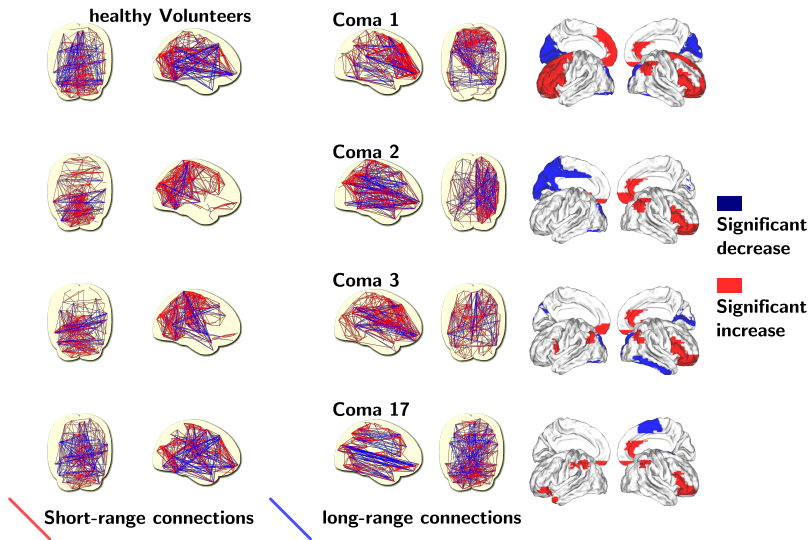
# A clinical example: brain connectivity for coma patients

## fMRI data acquisition parameters

- **90 and 417 anatomical regions:** space average of the fMRI time series over all voxels in 90 (AAL) and 417 regions
- **SPM preprocessing:** correction for geometrical displacements
- **Resting state:** lying quietly with eyes closed during 20 minutes
- **Group comparison:**  
20 young healthy volunteers, 17 patients in coma

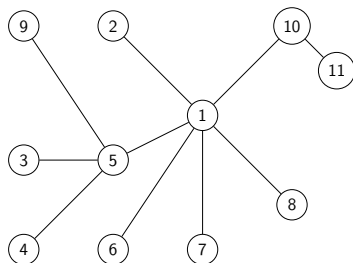
[Achard *et al.* PNAS 2012]

# Brain connectivity of coma patients

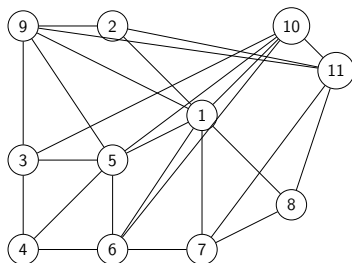


[Achard *et al.* PNAS 2012]

## Graph features: degree



low degree

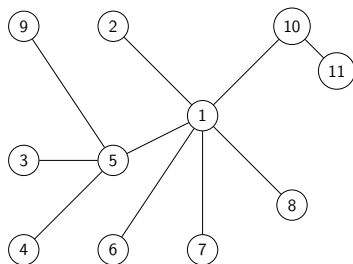


high degree

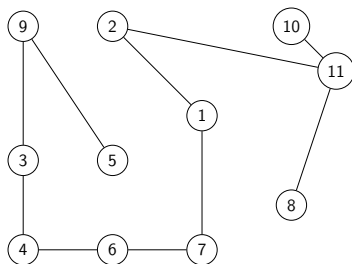
**Degree** = number of connections that node makes to other nodes.  
 $G = [G_{ij}]_{1 \leq i, j \leq N}$  is the adjacency matrix  $1 \leq i, j \leq N$ ,  $G_{ij} = 0$  or  $1$ .

$$D_i = \sum_{j \in G} G_{ij}.$$

## Graph features: global efficiency



Eglob close to 1



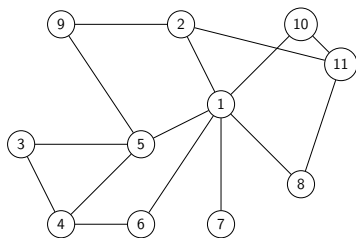
Eglob close to 0

**Efficiency** = inverse of the harmonic mean of the minimum path length  $L_{ij}$  between a node  $i$  and all the other nodes  $j$  in the graphs.

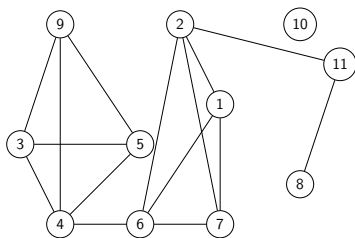
$$Eglob_i = \frac{1}{N-1} \sum_{j \in G} \frac{1}{L_{ij}}$$

[Latora et al. 2002]

# Graph features: clustering



Clust close to 0



Clust close to 1

**Clustering**, also called “local efficiency” = measure of information transfer in the immediate neighbourhood of each node.

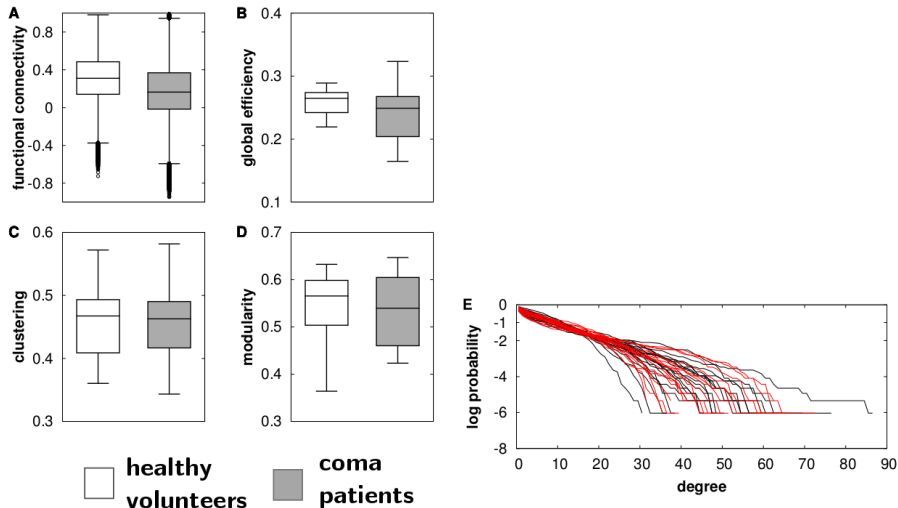
$$Clust_i = \frac{1}{N_{G_i}(N_{G_i} - 1)} \sum_{j,k \in G_i} \frac{1}{L_{jk}}$$

[Latora et al. 2002]



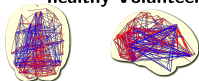
# Results: global connectivity and network topology

No significant difference on global measure of functional connectivity

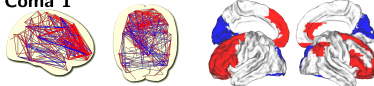


# Examples of connectivity graphs

healthy Volunteers



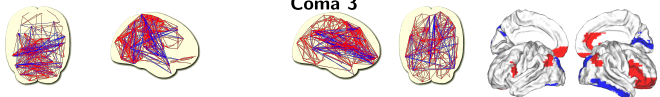
Coma 1



Coma 2



Coma 3



Coma 17



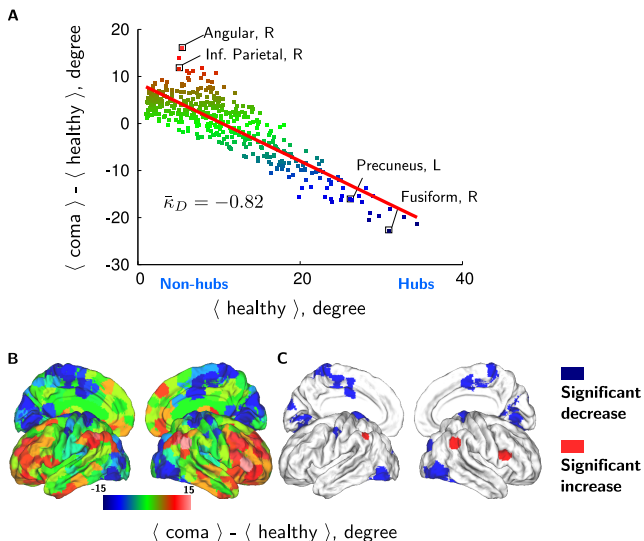
■ Significant decrease

■ Significant increase

Short-range connections

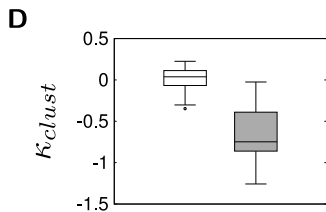
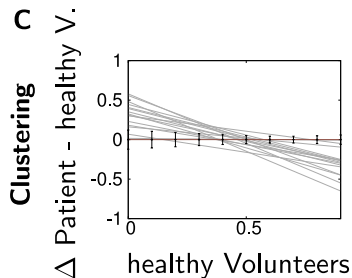
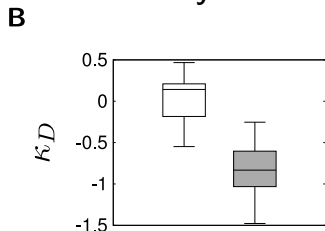
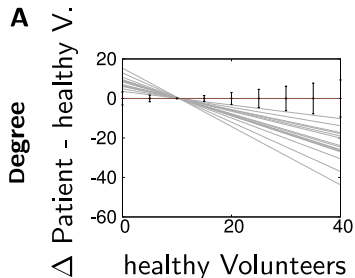
long-range connections

# Results: nodal connectivity



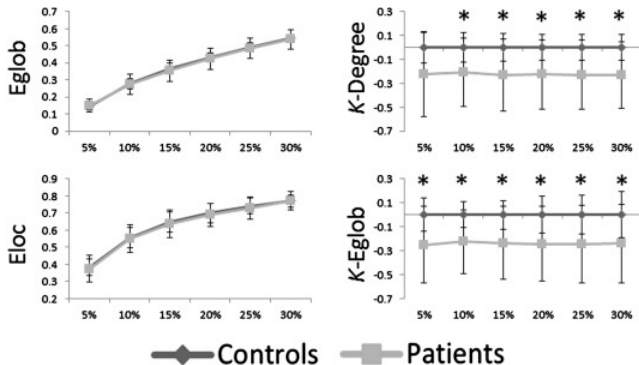
# Results: hub disruption index

One index to discriminate the coma and healthy volunteers



# Hub disruption index on epilepsy

Same results on epilepsy patients



[Ridley *et al.* Neuroimage 2015]

## Test-retest datasets

- Freely available data from **Human Connectome Project**
- **90 and 417 anatomical regions:** space average of the fMRI time series over all voxels in 90 (AAL) and 417 regions
- **SPM preprocessing:** correction for geometrical displacements
- **Resting state:** lying quietly with eyes closed during 20 minutes
- **Group comparison:**  
100 healthy controls scanned twice

[Termenon *et al.* Neuroimage 2012]

# Assessing reliability of graph analysis

Taking global efficiency as the metric studied and computed with the whole 1200 time points

$$ICC = \frac{s_b - s_w}{s_b + (k - 1)s_w} \quad (1)$$

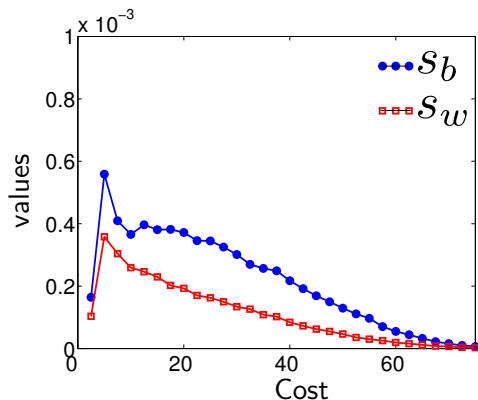
where  $s_b$  is the variance between subjects,  $s_w$  is the variance within subjects and  $k$  is the number of sessions per subject.

[Fisher *et al.* 1925] [Donner *et al.* 1986]

# Assessing reliability of graph analysis

Taking global efficiency as the metric studied and computed with the whole 1200 time points

For the 100 healthy volunteers scanned twice

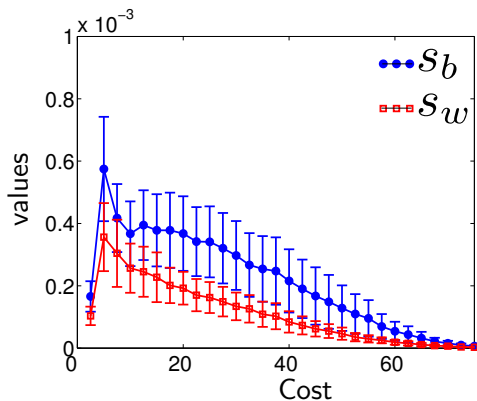




# Assessing reliability of graph analysis

Taking global efficiency as the metric studied and computed with the whole 1200 time points

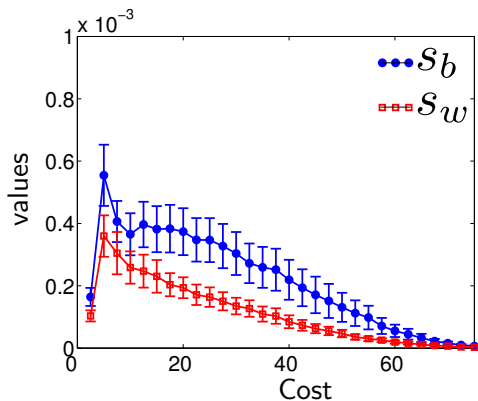
For 20 healthy volunteers taken at random using subsampling



# Assessing reliability of graph analysis

Taking global efficiency as the metric studied and computed with the whole 1200 time points

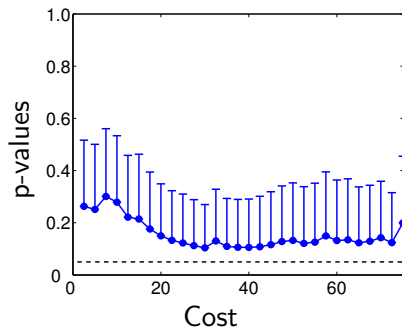
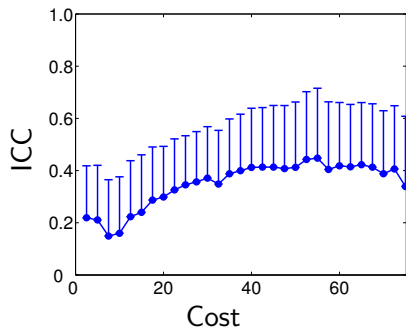
For 40 healthy volunteers taken at random using subsampling



# Assessing reliability: p-values of ICC

Permutation tests to compute p-values

For 20 subjects, 1200 time points, global efficiency

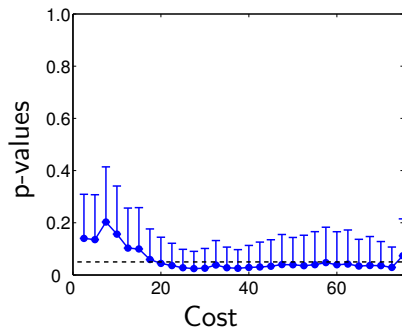
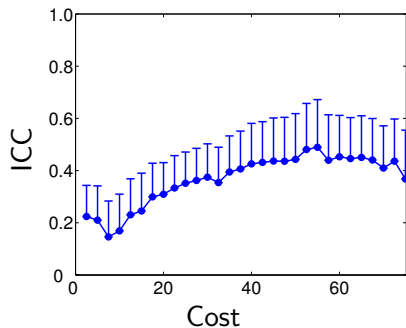


Simctest [Gandy *et al.* 2009]

# Assessing reliability: p-values of ICC

Permutation tests to compute p-values

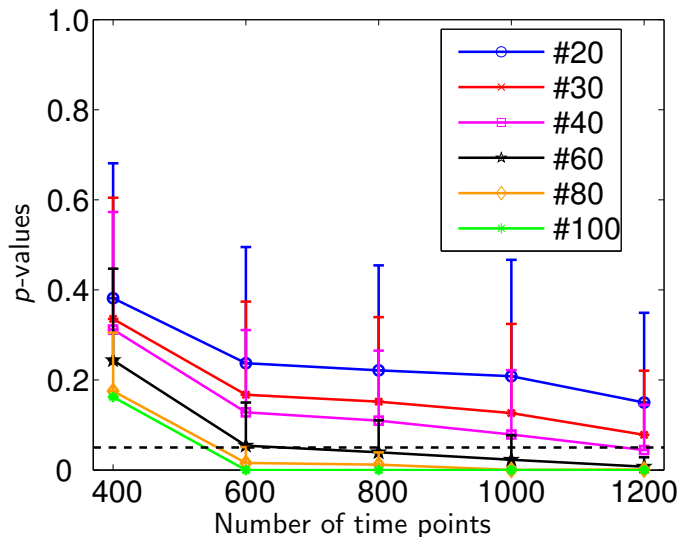
For 40 subjects, 1200 time points, global efficiency



Simctest [Gandy *et al.* 2009]

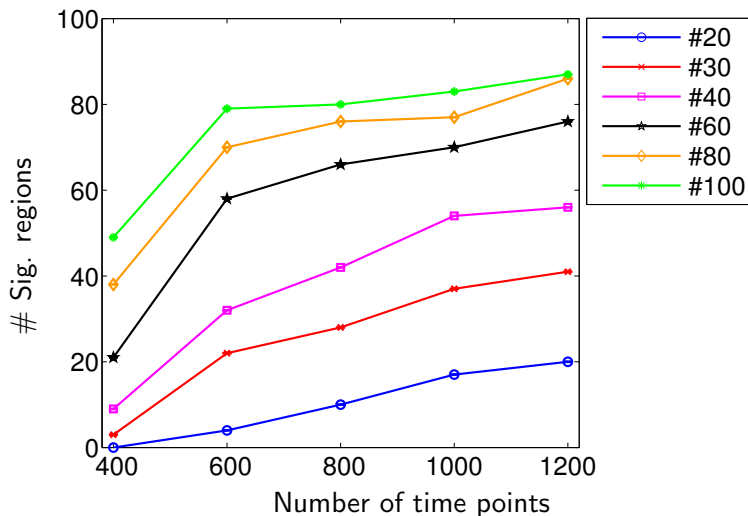
# Choice of number of subjects and scan duration

Comparisons for global efficiency for a cost equal to 20%

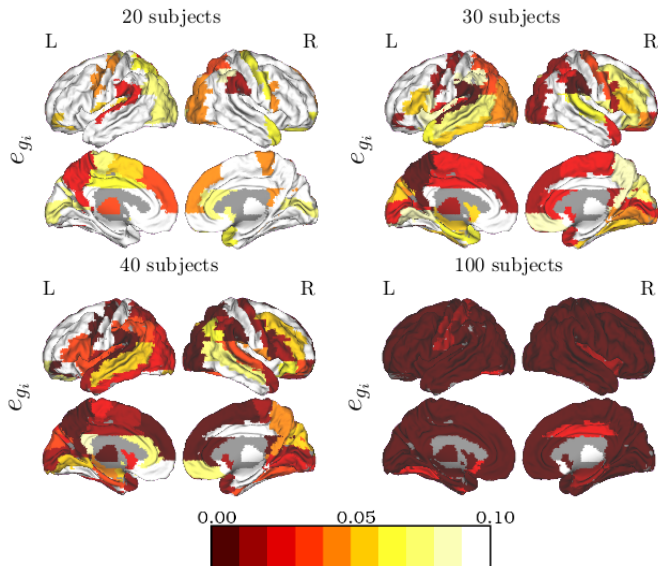


# Significant regions versus number of subjects

At the regional level, global efficiency of each region separately



# Localisation of significant regions



## Conclusions and future works

- Graphs are providing a complete representation of brain connectivity
- New graph metrics are needed
- Assessing reliability is worthwhile for any new approaches

Feel free to use the test-retest datasets  
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# Thanks to my collaborators

